



Second-level analysis of PET and MRI data

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Basic problems associated with scientific measurement

ERRORS PRESENT AT ALL LEVELS; THEY ALSO ACCUMULATE FROM LEVEL TO LEVEL

TARGET
(e.g. specific neuro-receptor)

TRUE SCORE (T)
How target is defined
(e.g. number of receptors)

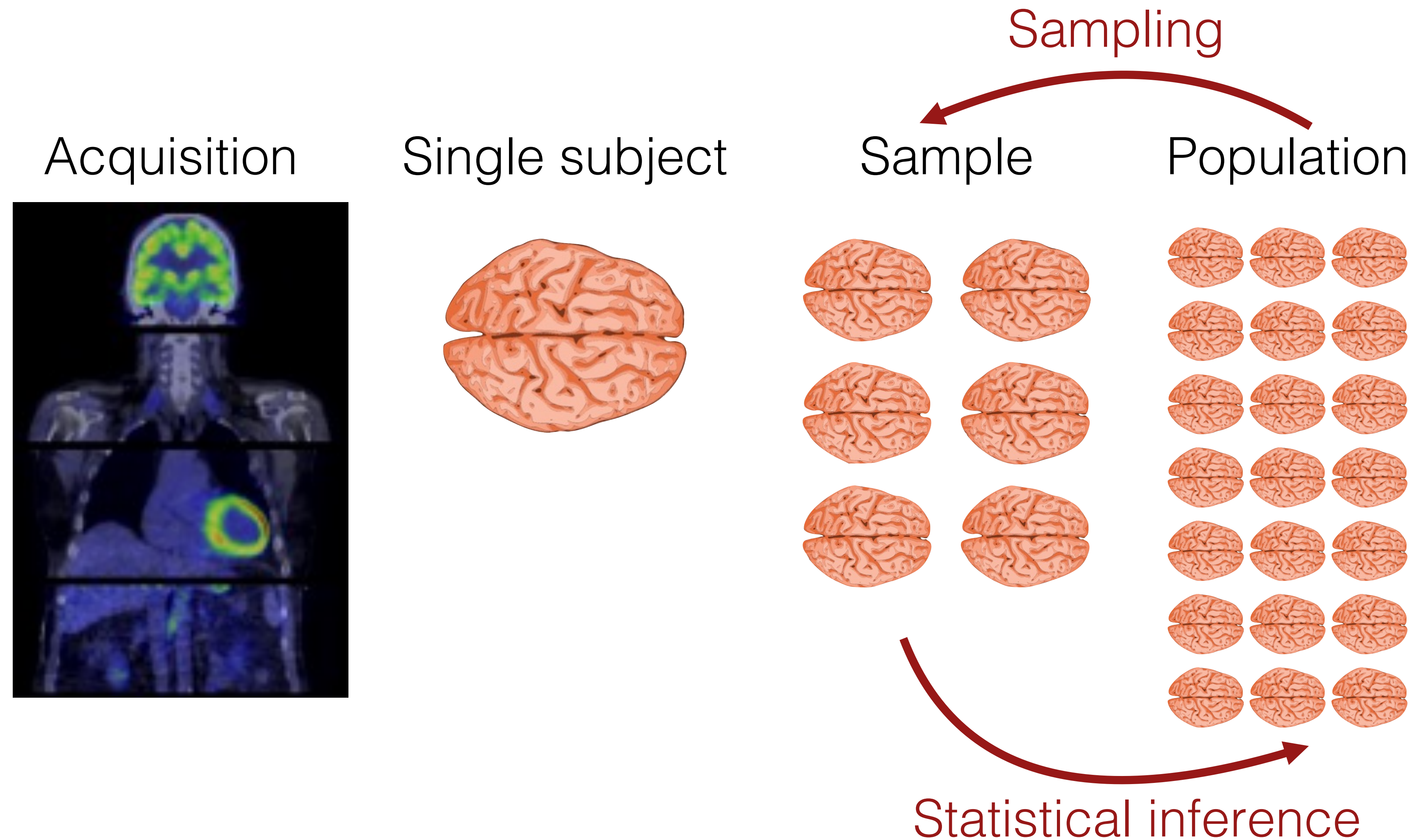


OBSERVED SCORE
(Outcome measure such as BPND)

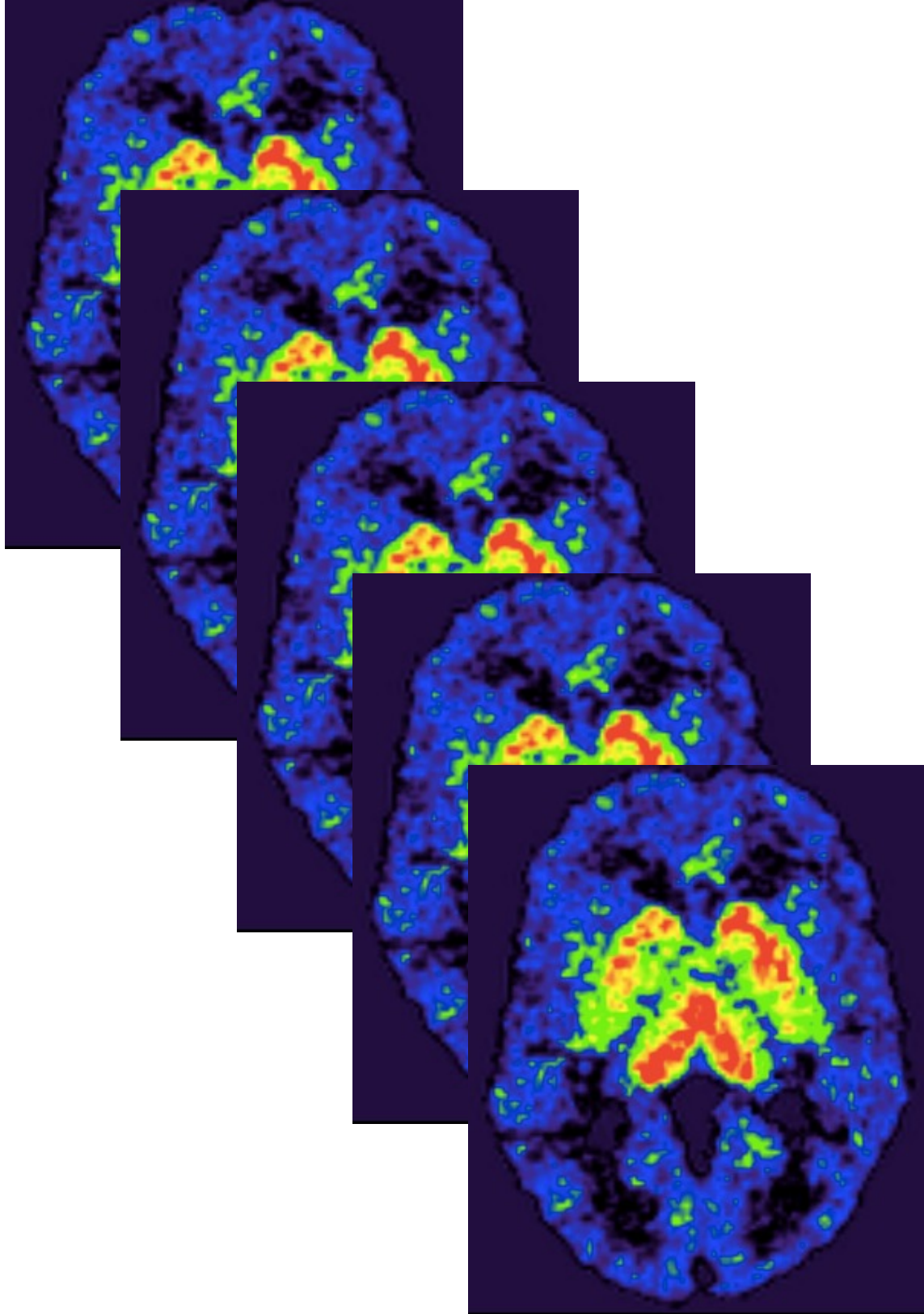
PREDICTION OF BEHAVIOR
(e.g. anxiety-like behaviour)

- How well is target variable reflected in true score (construct validity)
- How well true score is reflected in observed score? (reliability)
- How well does observed score predict behaviour? (criterion-based validity)

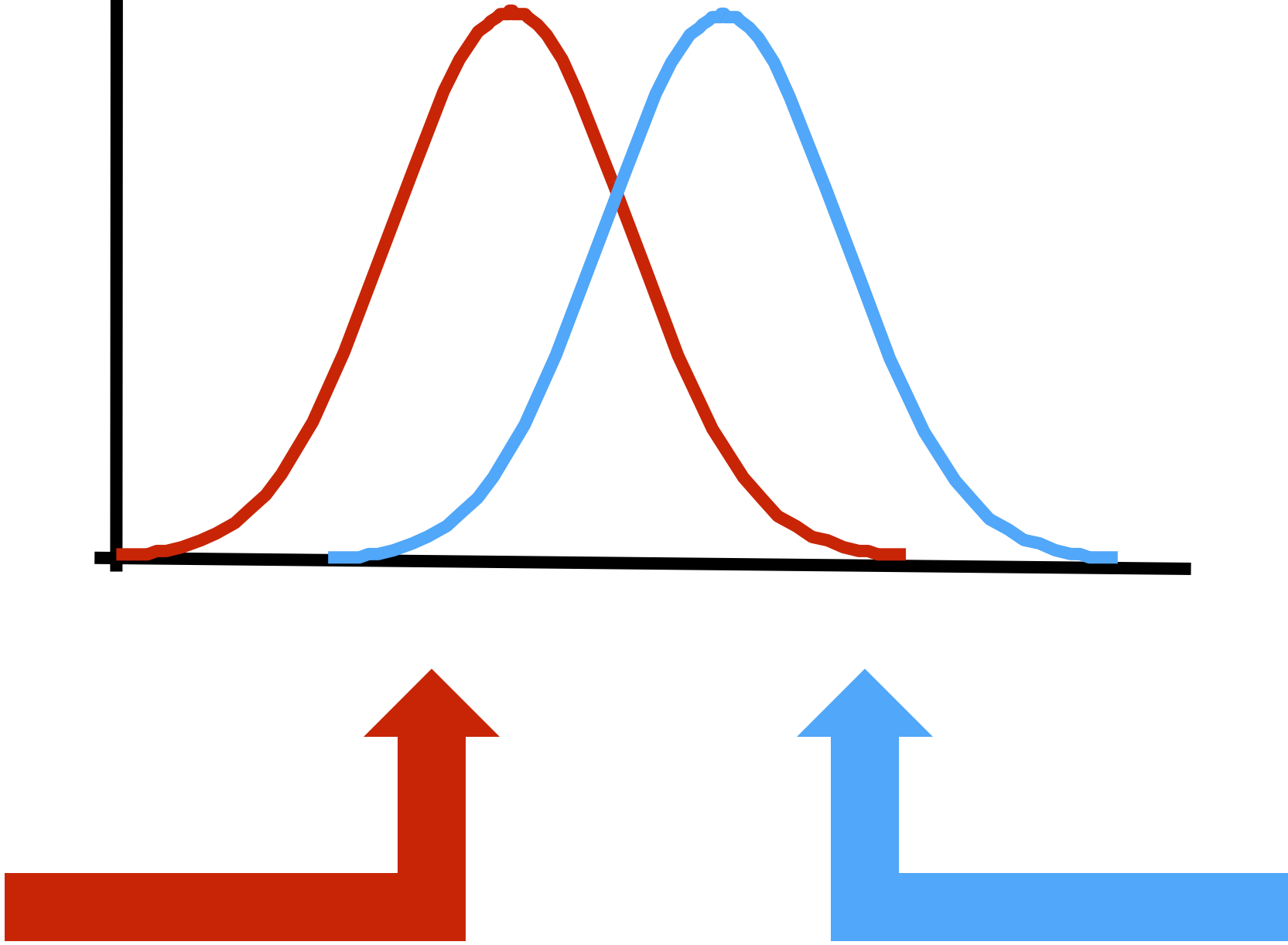
Making inferences about the population



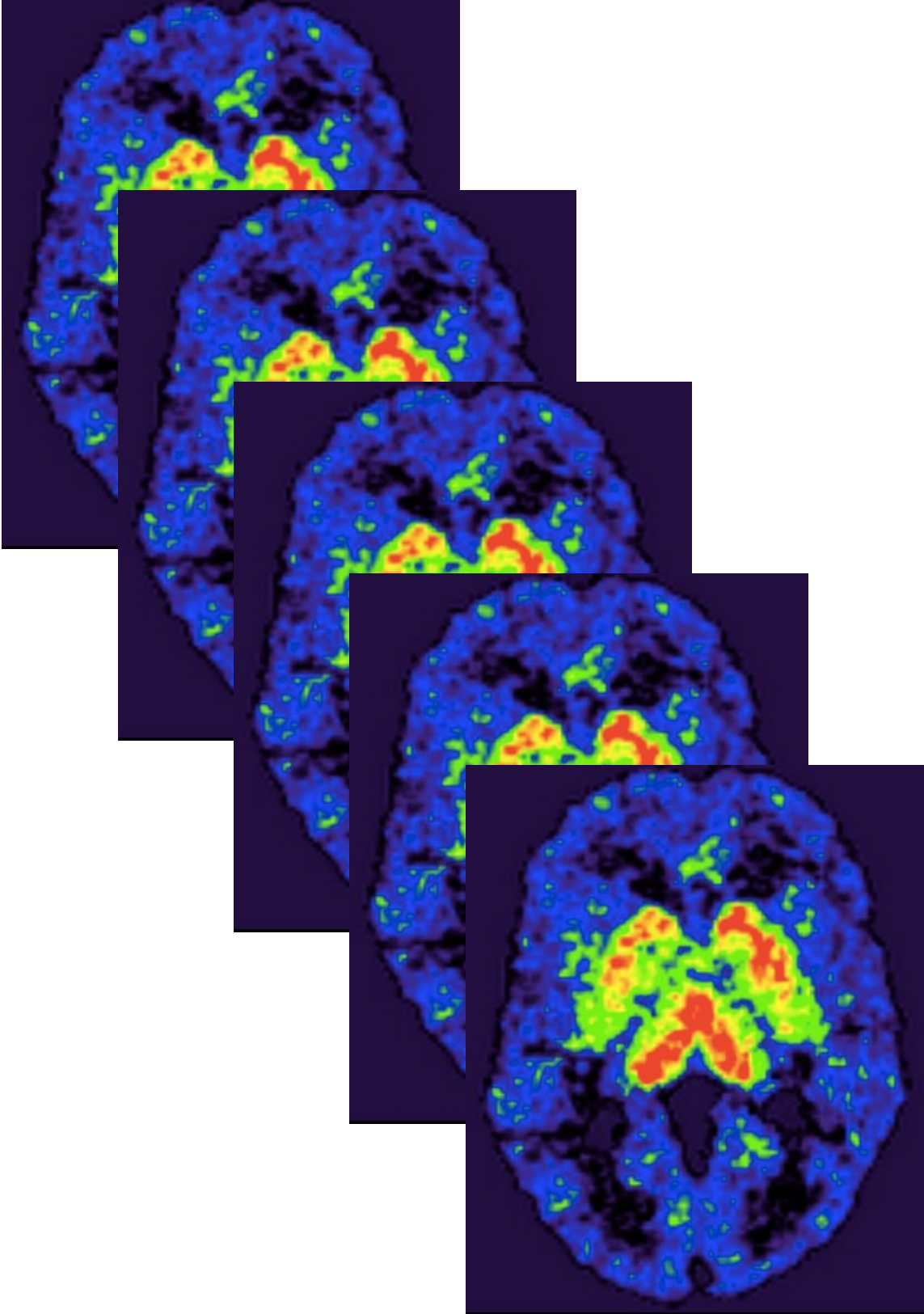
CONTROLS



ARE THESE BRAINS
STATISTICALLY
DIFFERENT?



PATIENTS

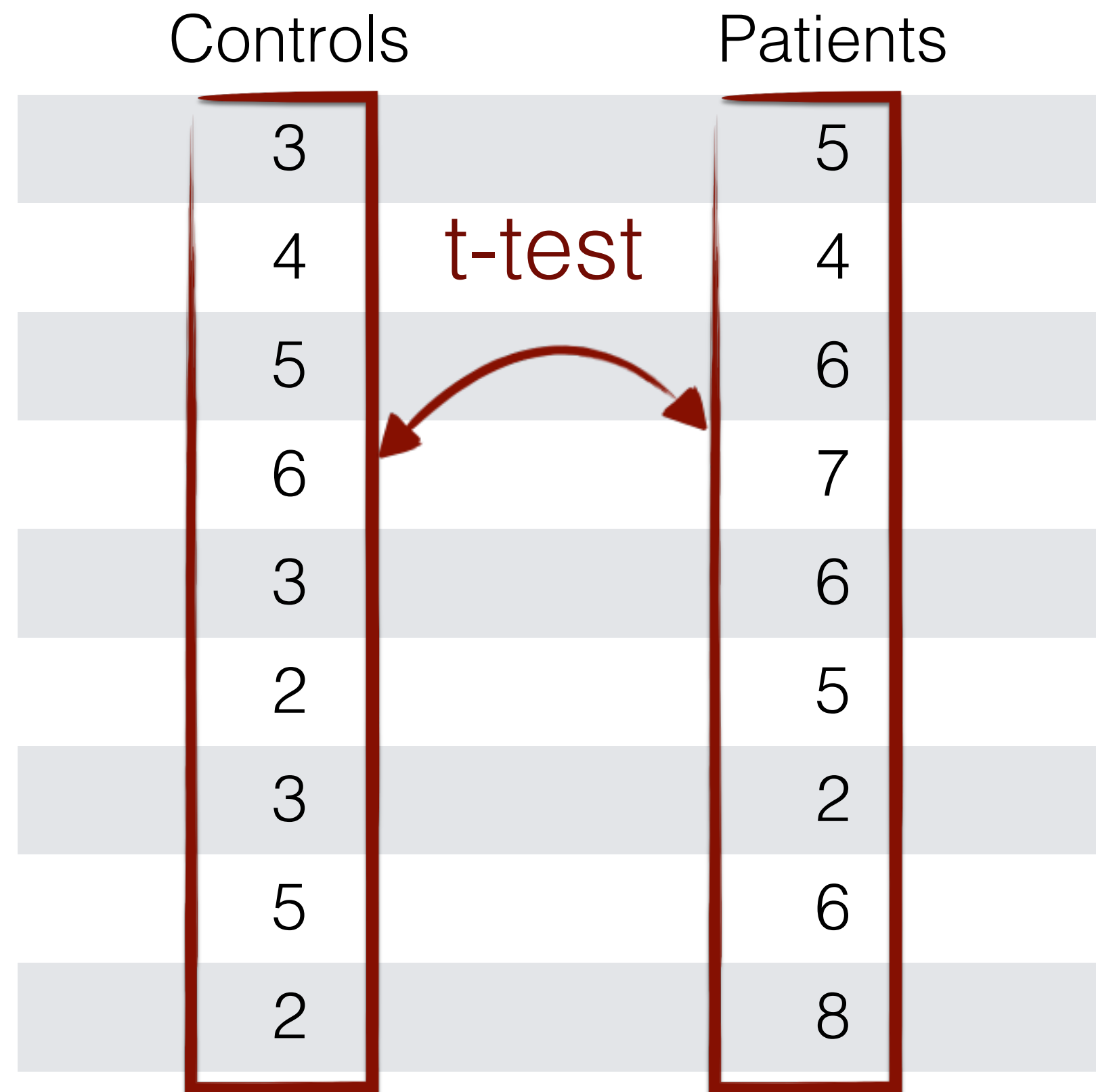


Starting point: Images where voxel intensities reflect the outcome measure

Sneak peek: Analysis of PET vs. fMRI data

- **PET data needs to be modelled** before population level inference
 - 4D image \rightarrow 3D image
 - Voxel intensities reflect outcome measure (receptor density, metabolism....)
- **Similarly, EPI data needs to be modelled** before population level inference
 - 4D image \rightarrow 3D image
 - Voxel intensities reflect the fit of the stimulation model to the BOLD time series

Univariate data
Regularly shaped

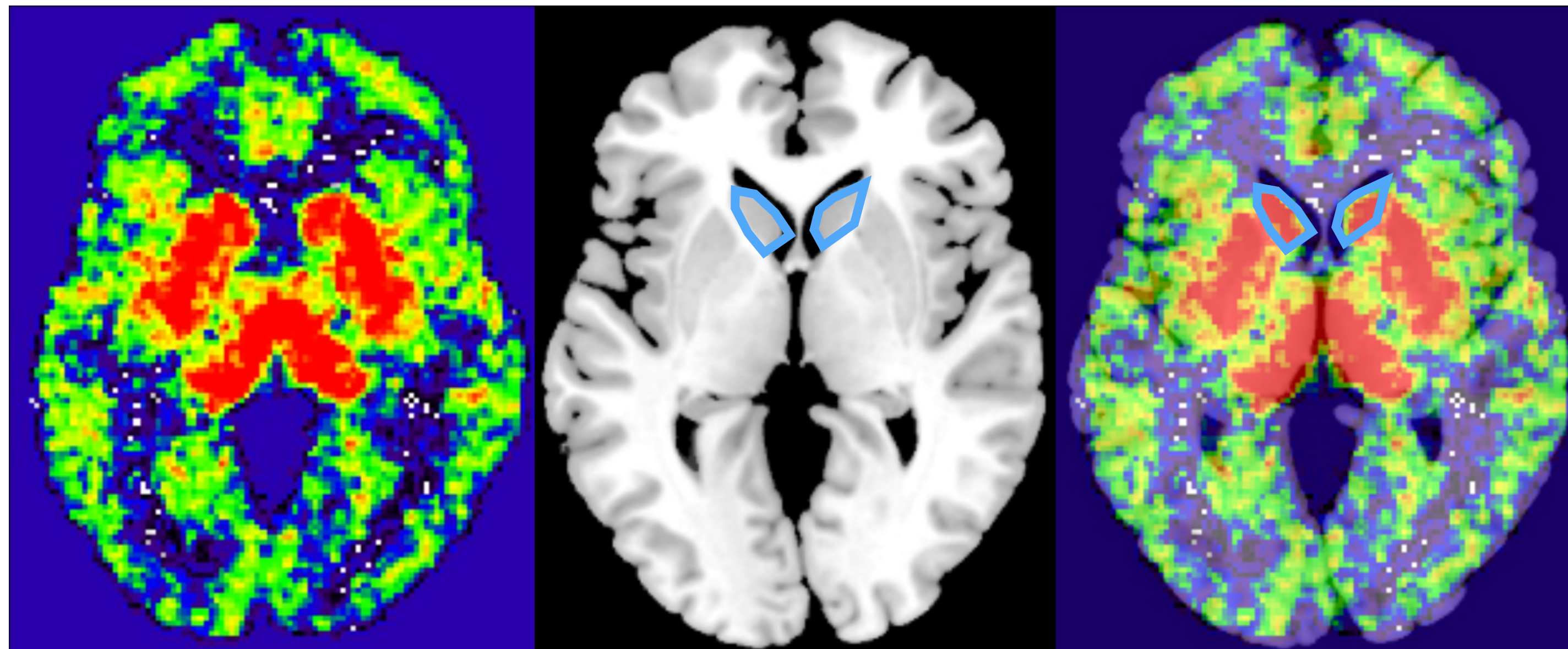


3D neuroimaging data
Irregularly shaped



ROI-based analyses

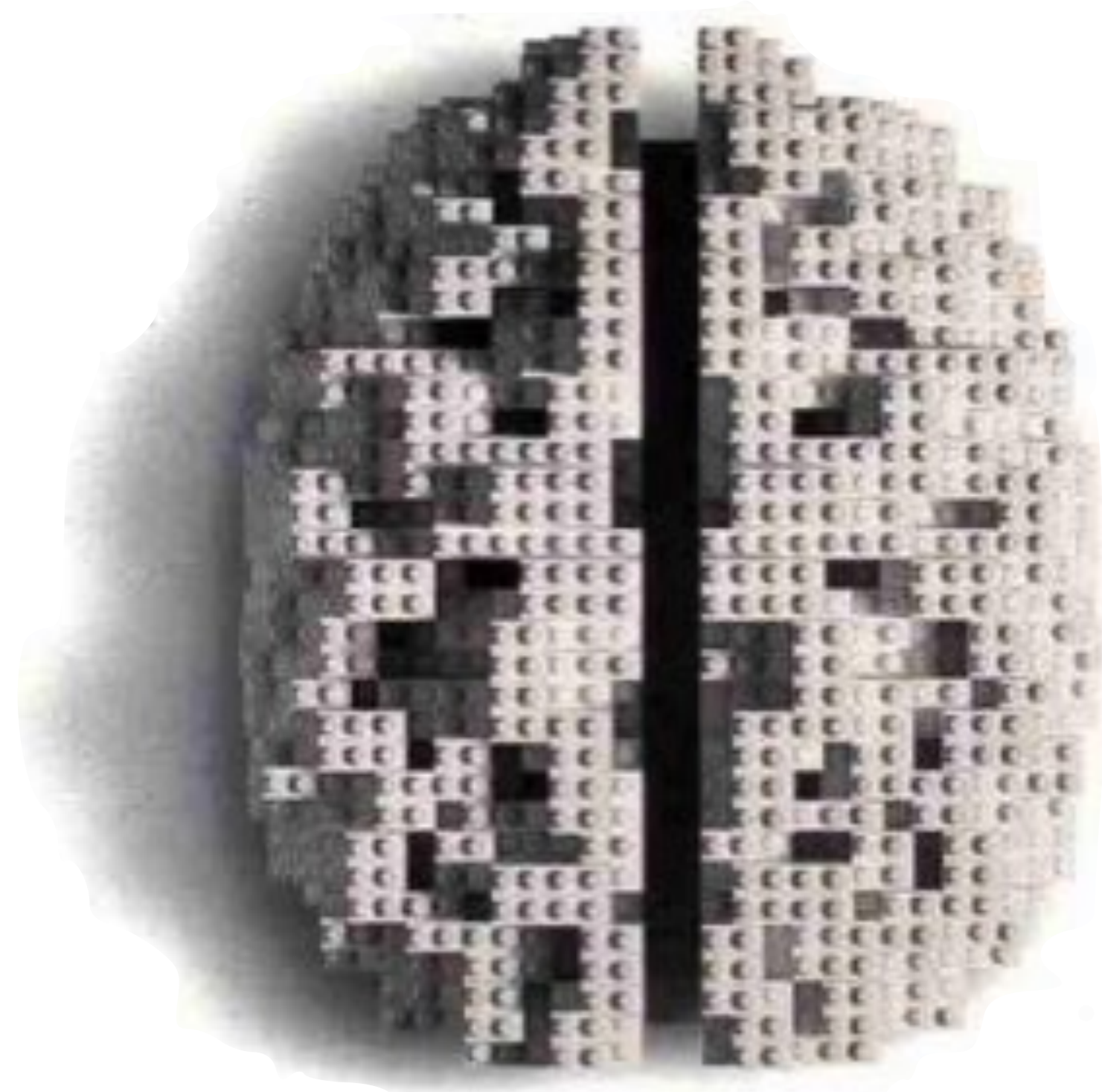
Univariate data
regularly shaped
can use univariate stats

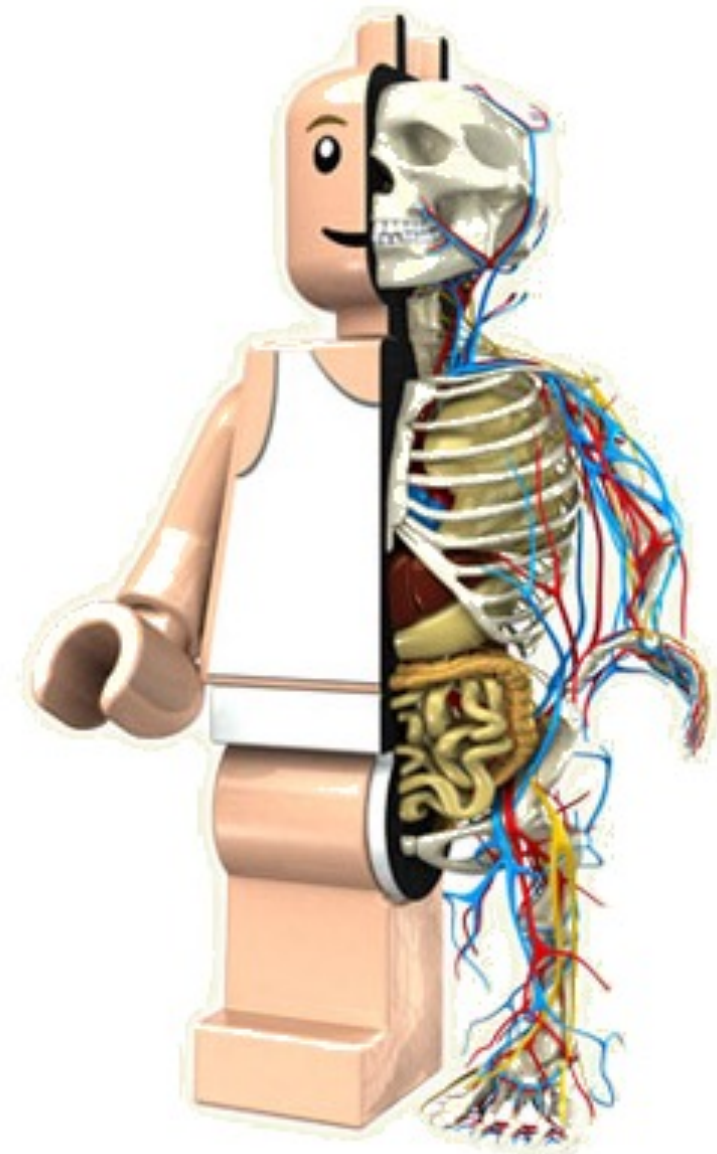


Extract
outcome
measure
in ROI

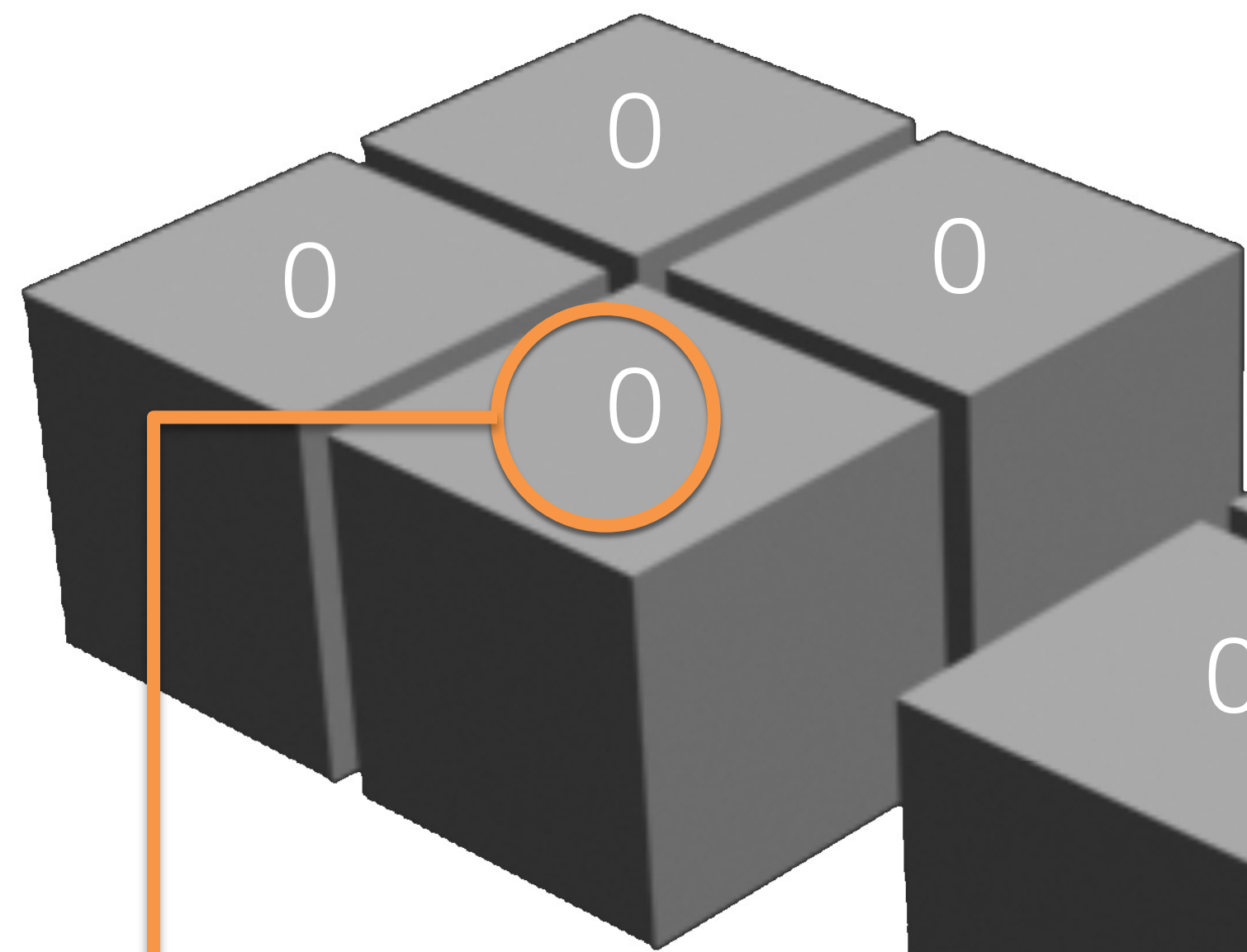
Controls	Patients
3	5
4	4
5	6
6	7
3	6
2	5
3	2
5	6
2	8

- **Pros:** Anatomically accurate if ROIs well defined, data can be analyzed with simple univariate statistical tests
- **Cons:** Laborious, using many ROIs not feasible, averaging within ROI not always appropriate





Controls

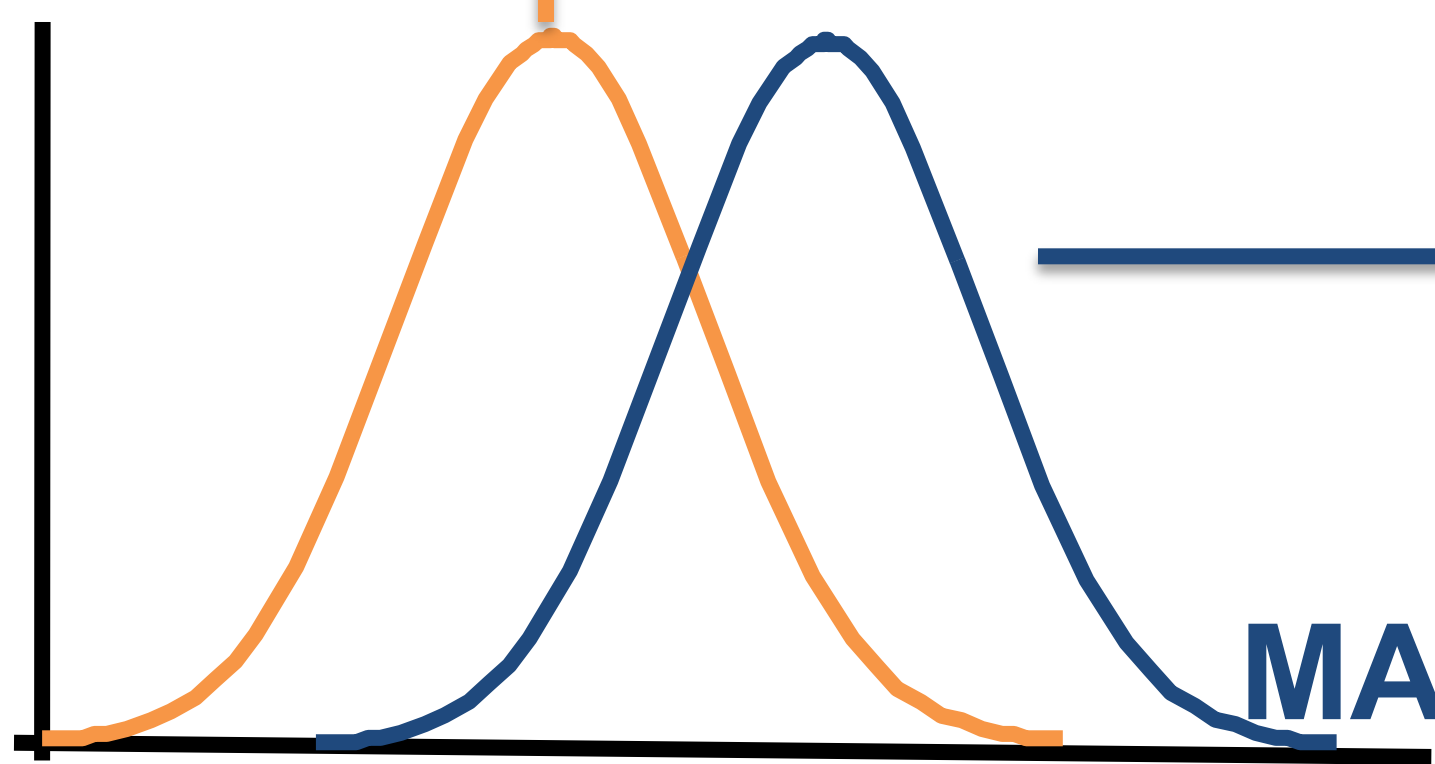
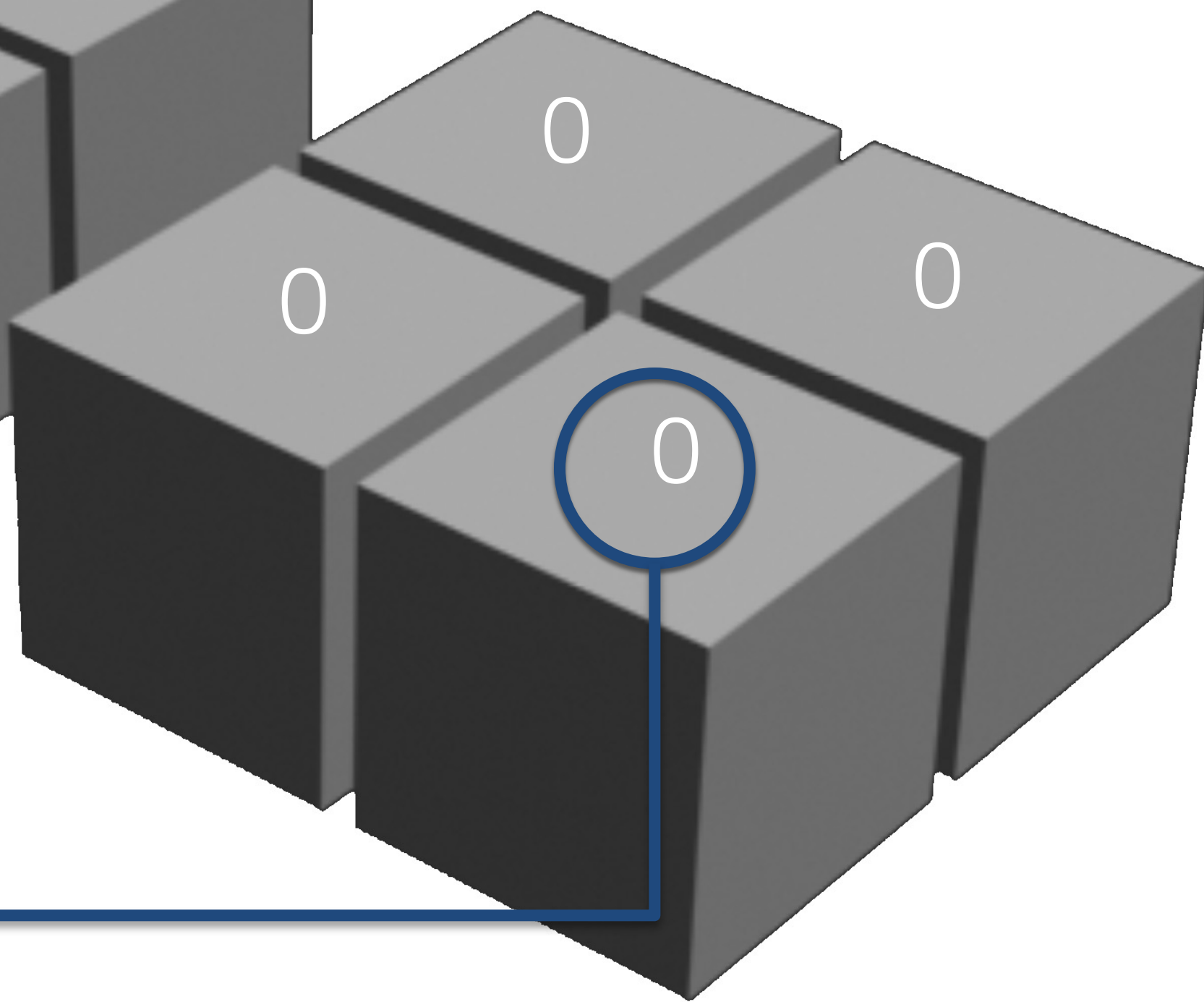


Voxelwise
outcome
measures



Univariate voxelwise data
regularly shaped
can use mass
univariate stats

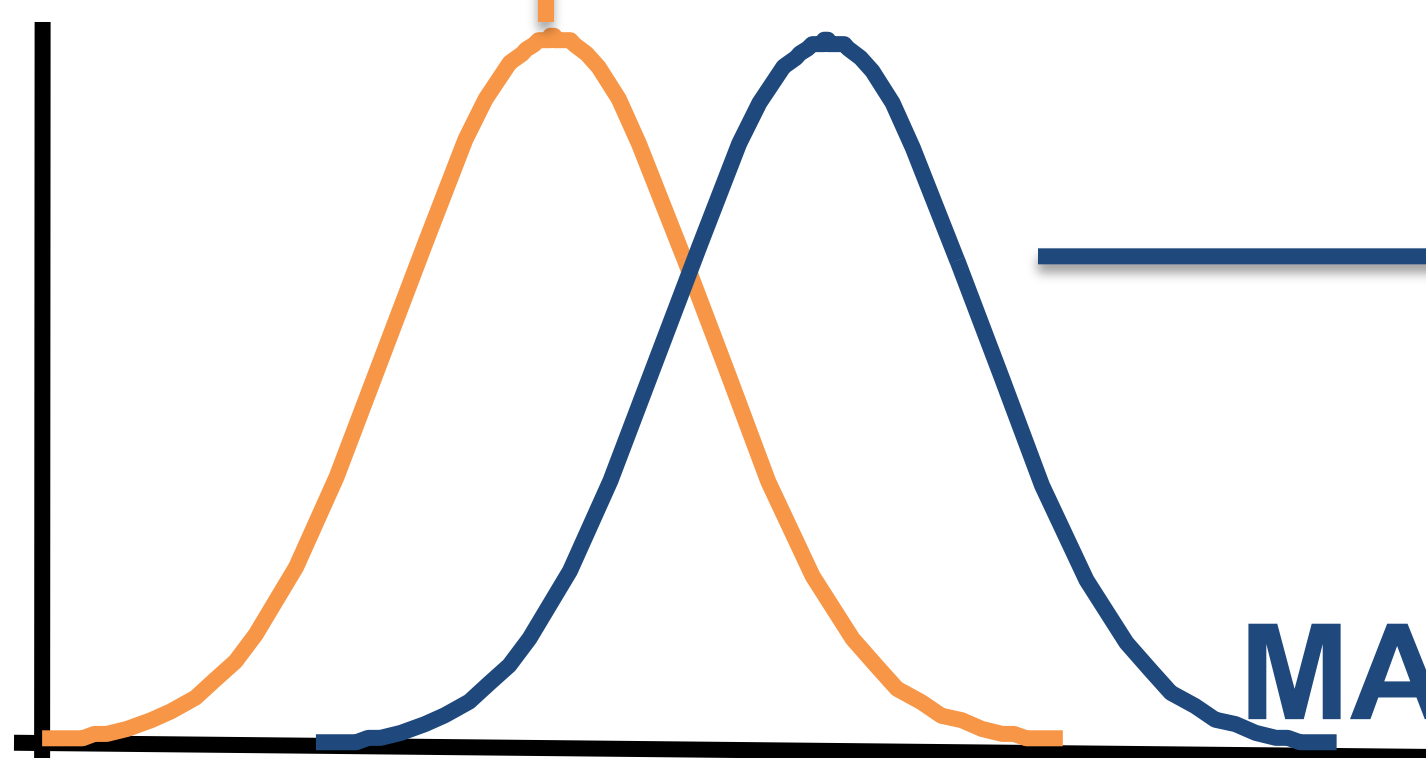
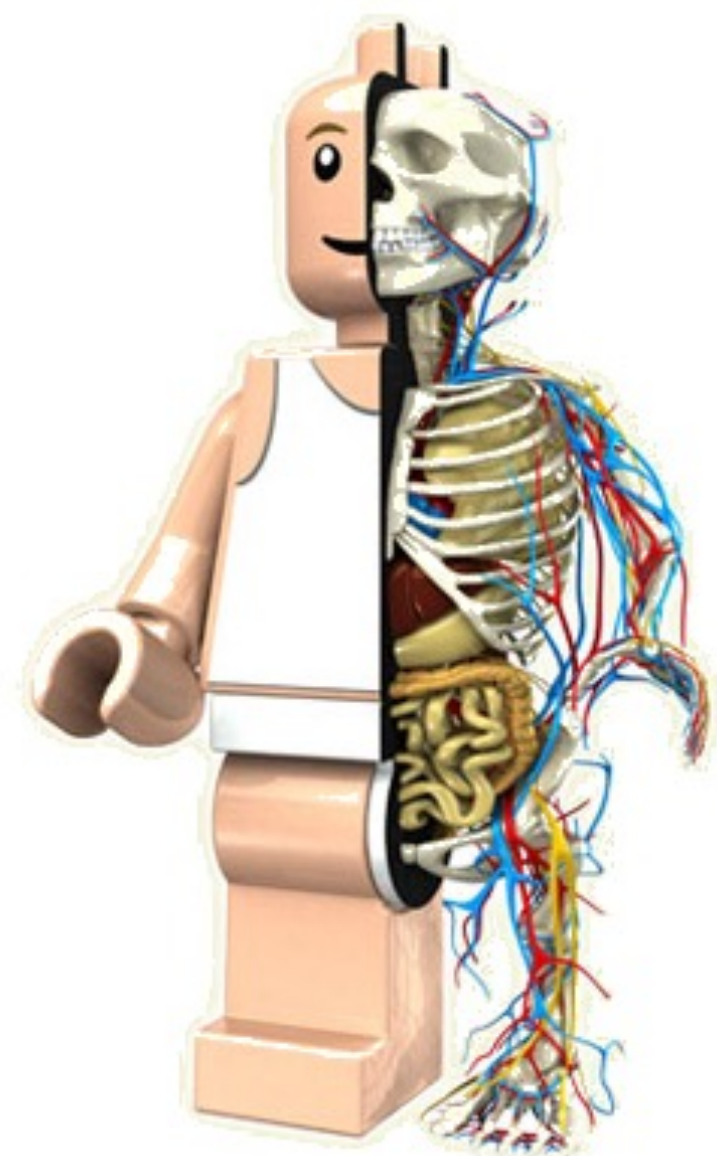
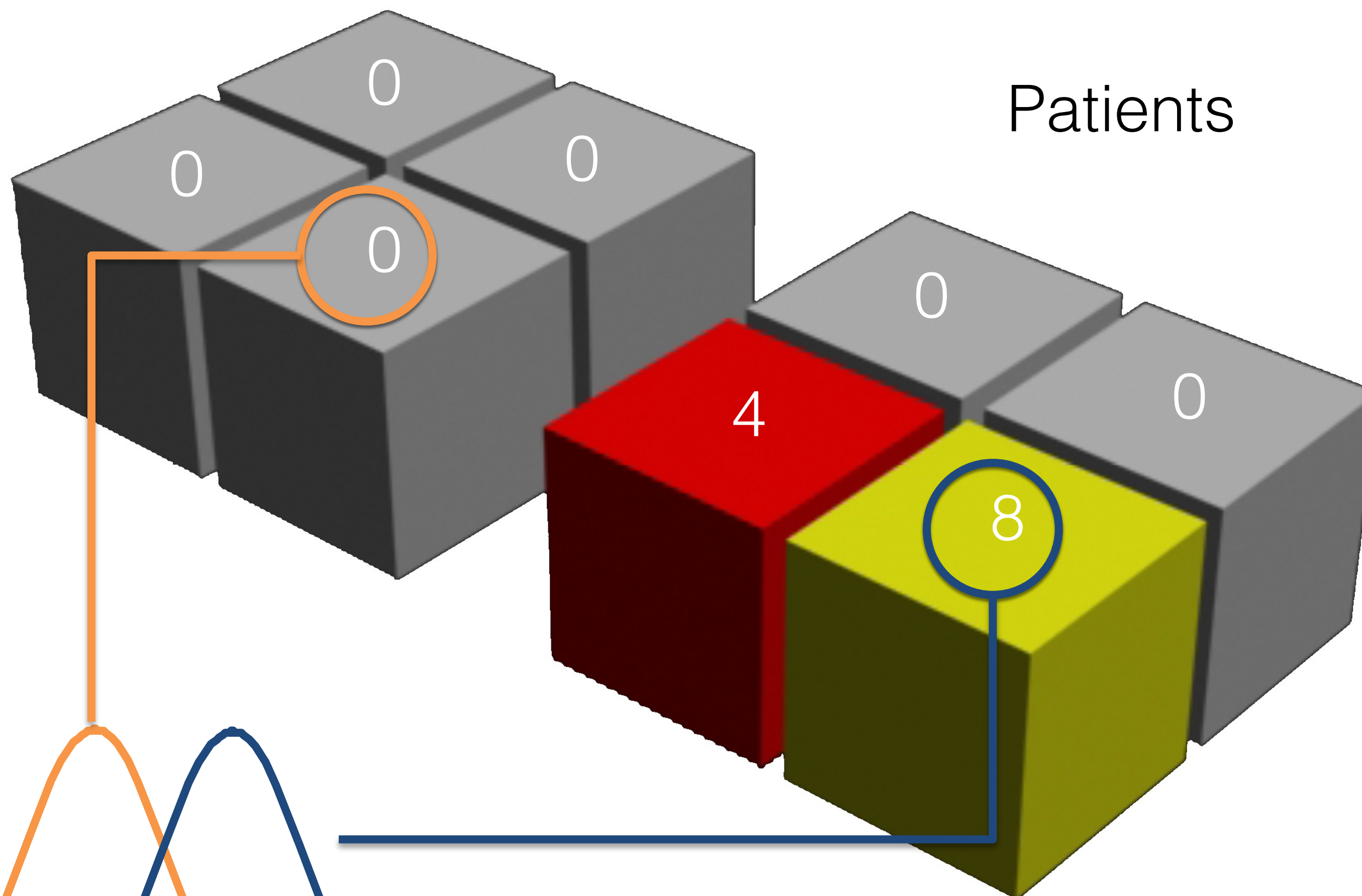
Patients



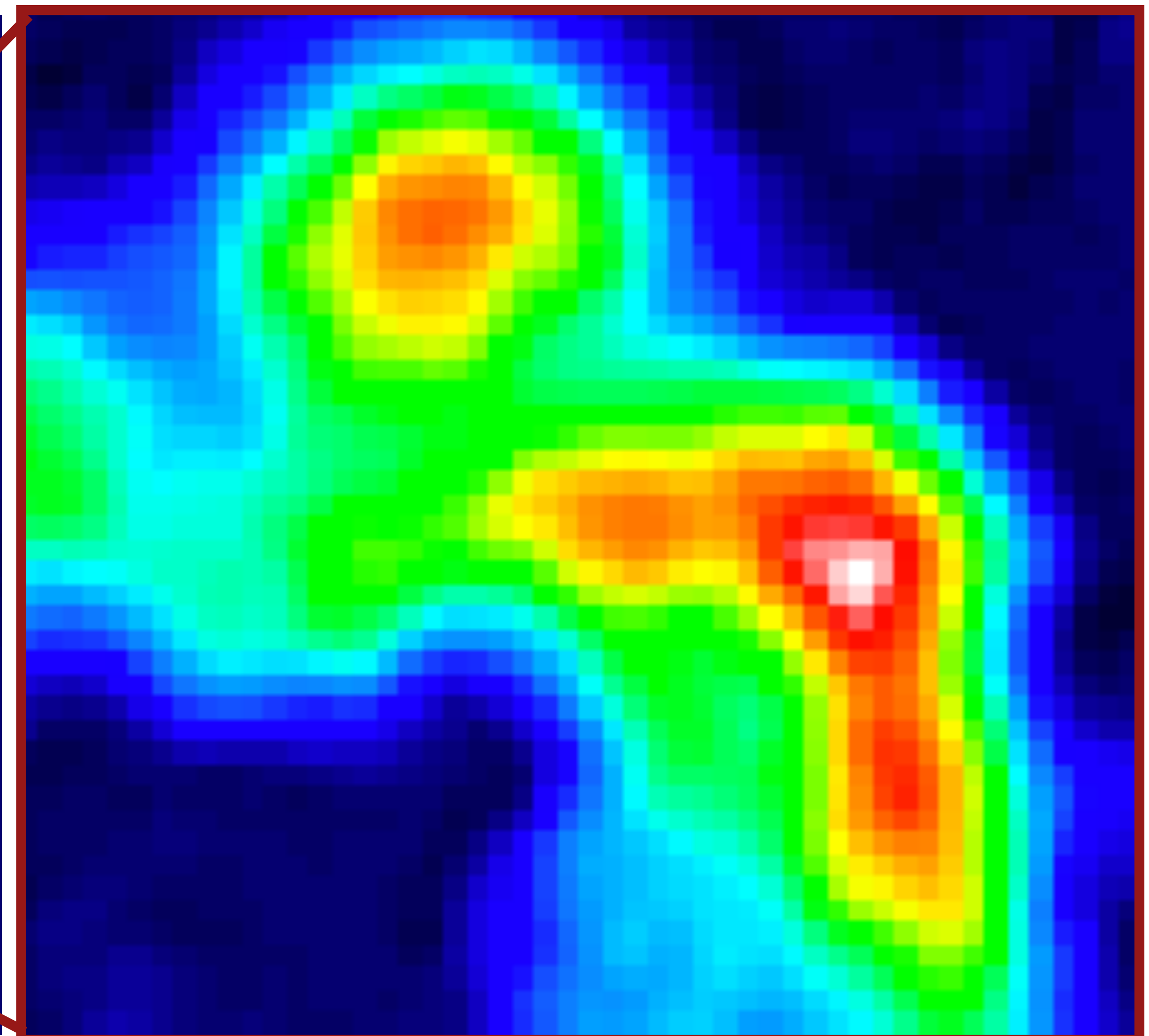
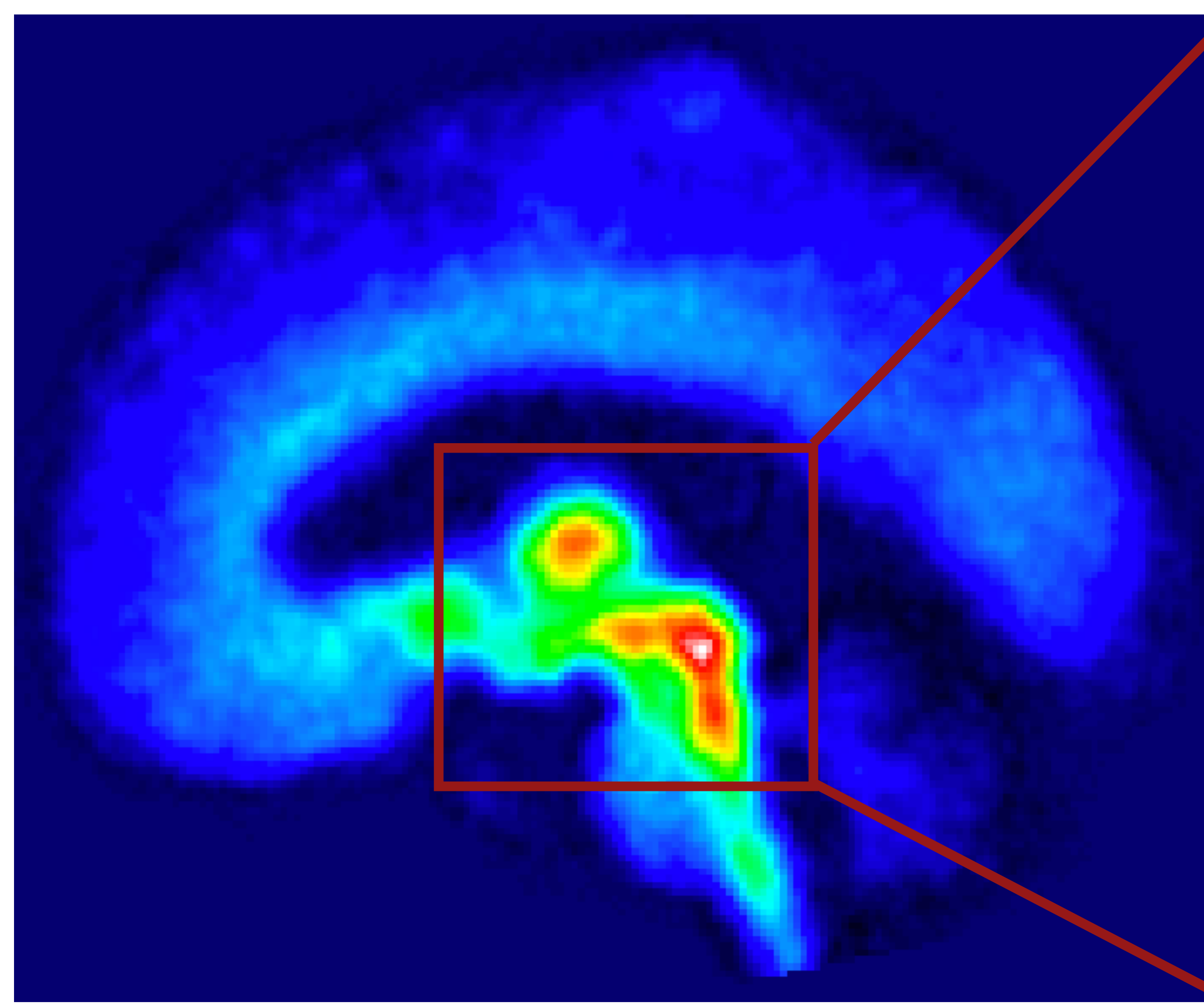
MASS UNIVARIATE TESTING FOR ALL VOXELS

Controls

Patients



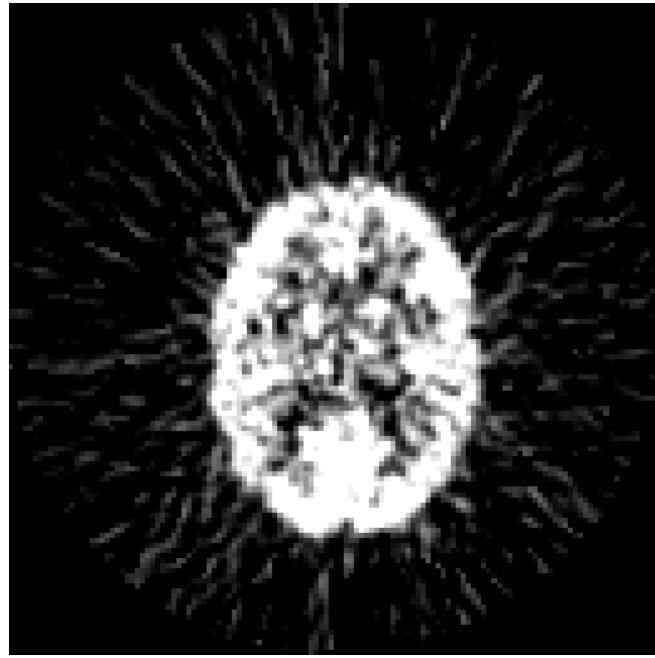
MASS UNIVARIATE TESTING FOR ALL VOXELS



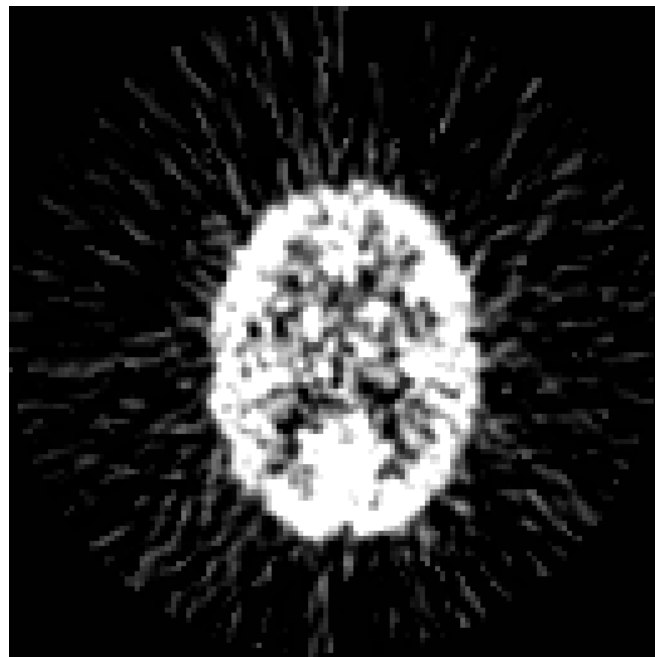
THE BASIC RECIPE

Voxel intensity = outcome measure
(BPND, contrast estimate, tissue probability)

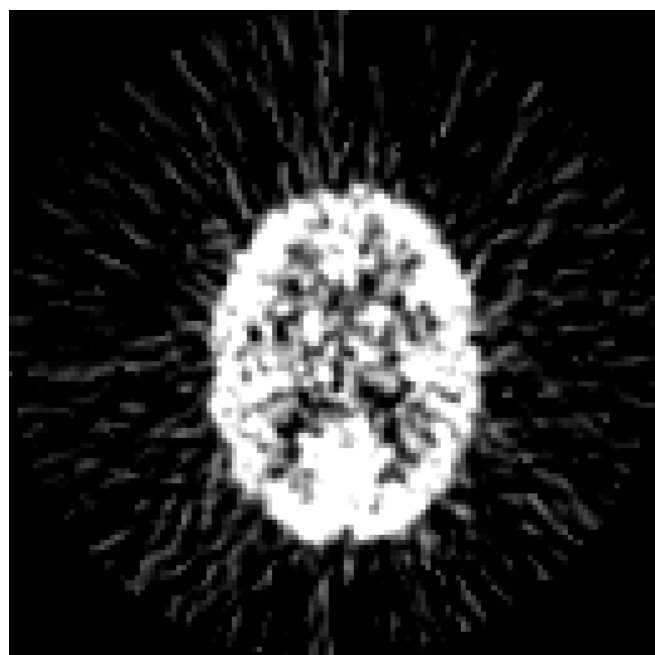
SUBJECT 1



SUBJECT 2

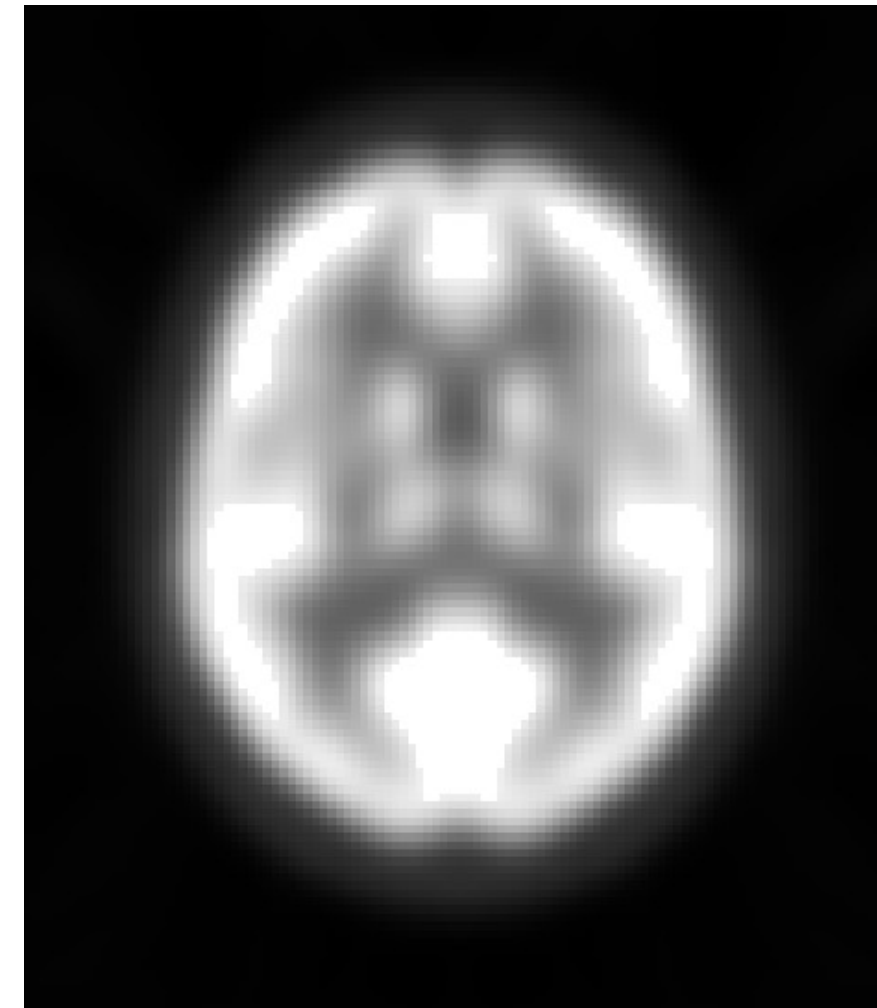


SUBJECT 3



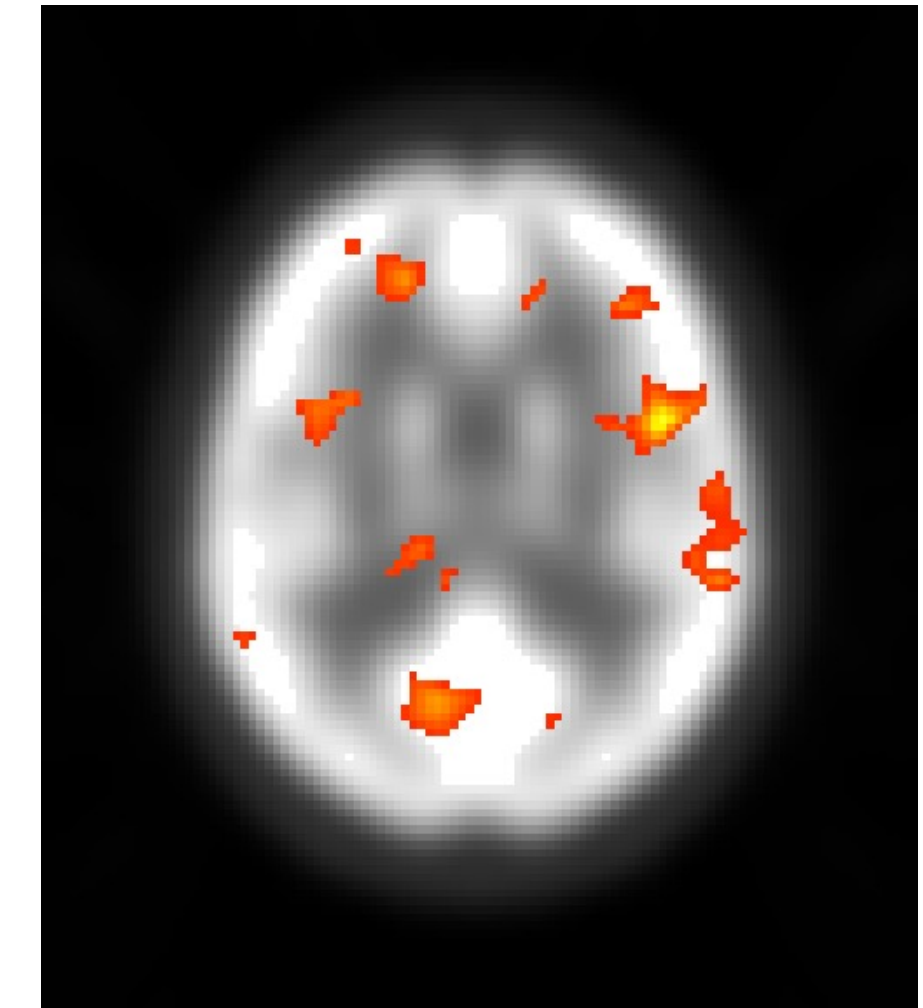
NORMALI-
ZATION

TEMPLATE

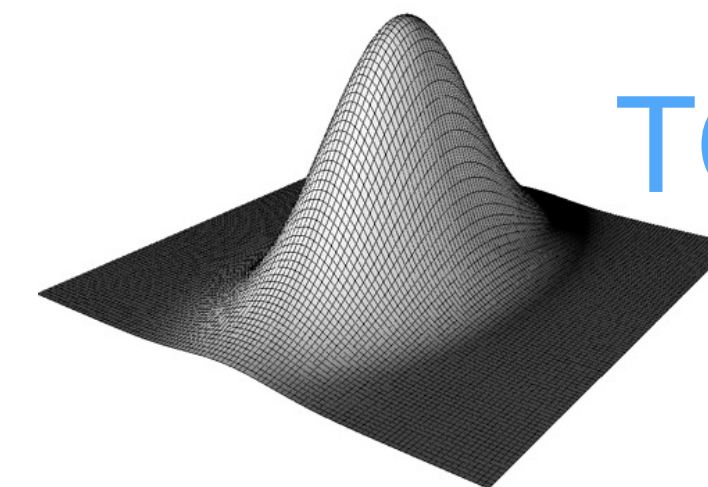


STATISTICAL
PARAMETRIC MAP

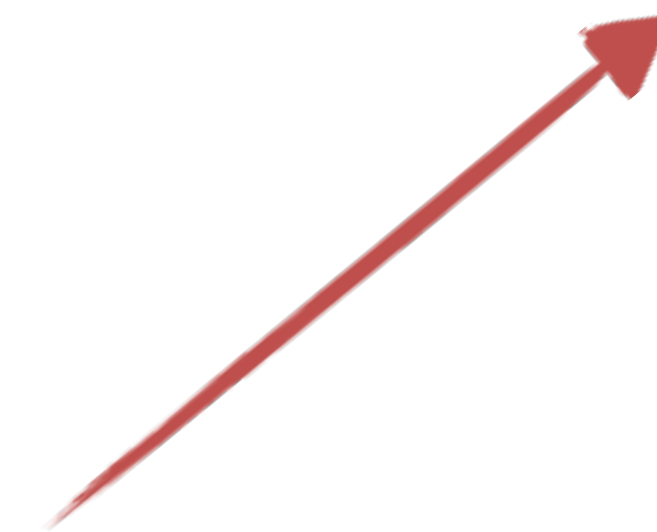
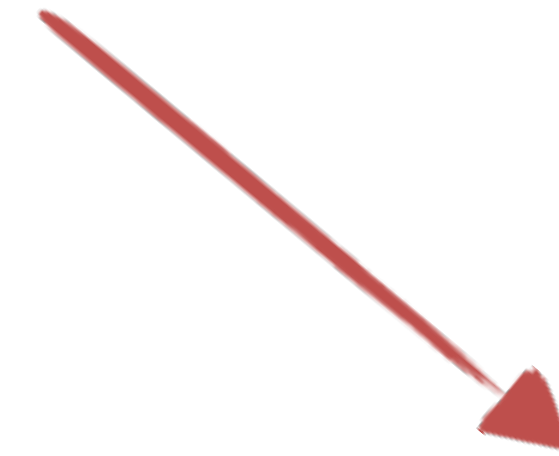
GLM



SMOOTH



THRESHOLD
TO HIGHLIGHT

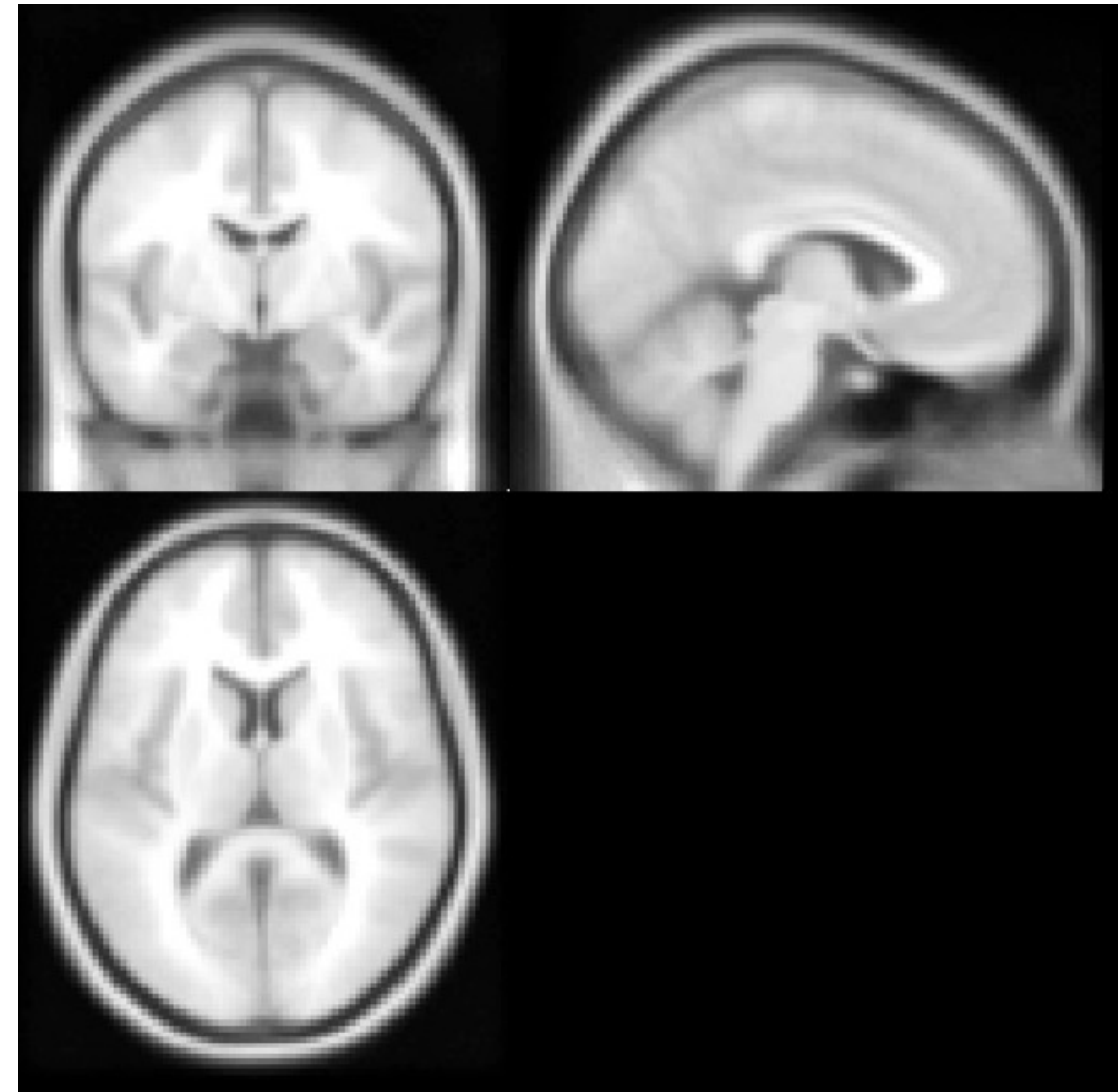


Full-volume analyses with real brains

- Basic problem: Individual brains differ in size and shape
- Solution to the problem: Make brains similar by warping them
- Problems with the solution
 - Warps distort anatomy
 - Anatomical information is not the precise anyway
 - How should we warp the brains?

The MNI space as the target

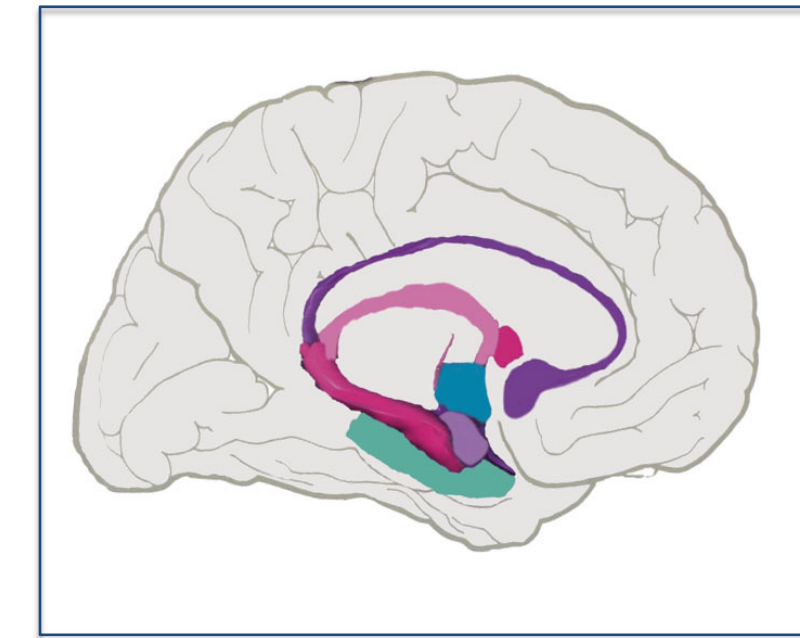
- **ICBM 152 template**
- Based on average of 152 brains that have been spatially normalized
- Statistical average of the typical western adult brain
- Problem: not necessarily representative of study sample
- In fMRI can also use e.g. spherical models



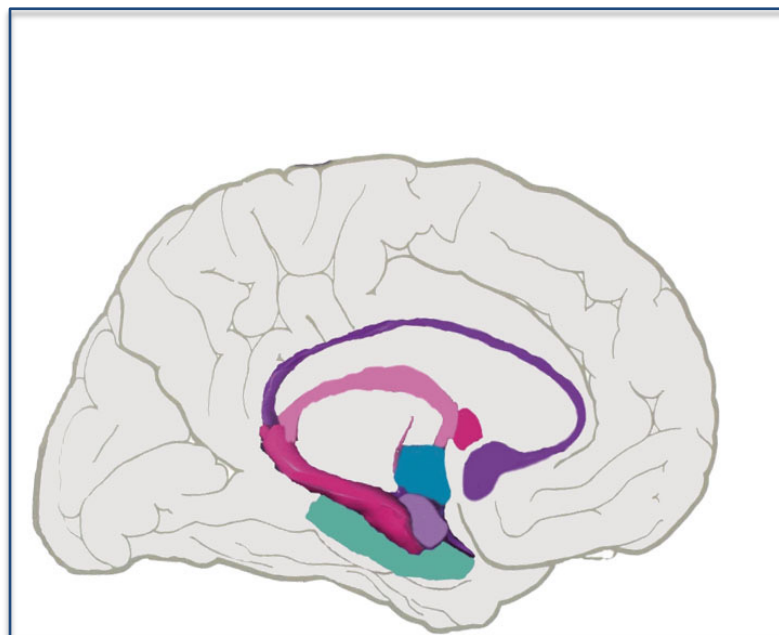
Spatial normalization in practice

1. Linear (12-parameter affine) normalization
 - Match size and position
2. Nonlinear normalization
 - Linear combinations of smooth discrete cosine basis functions

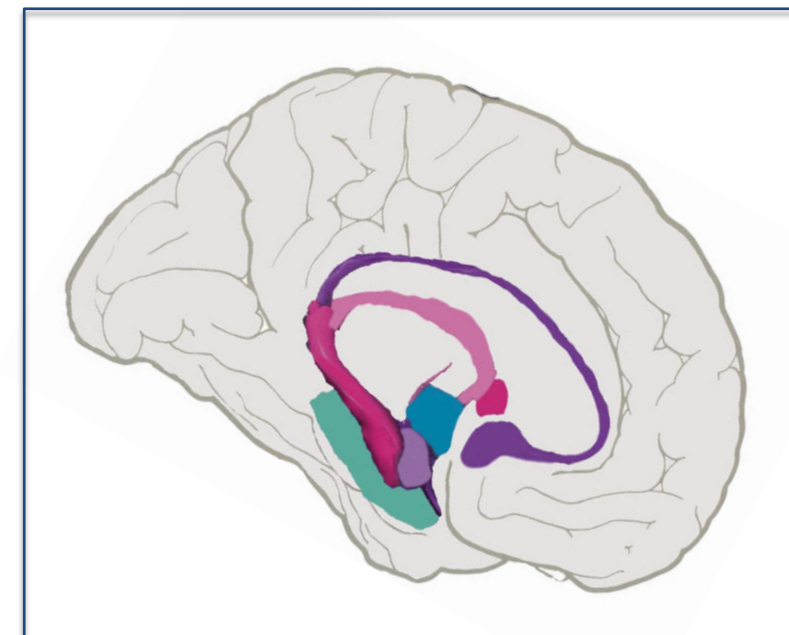
NATIVE



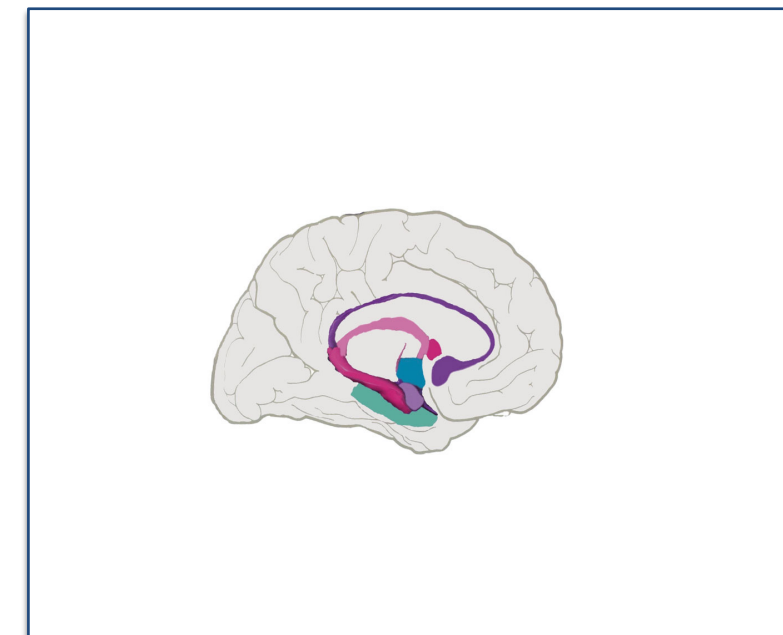
TRANSLATION



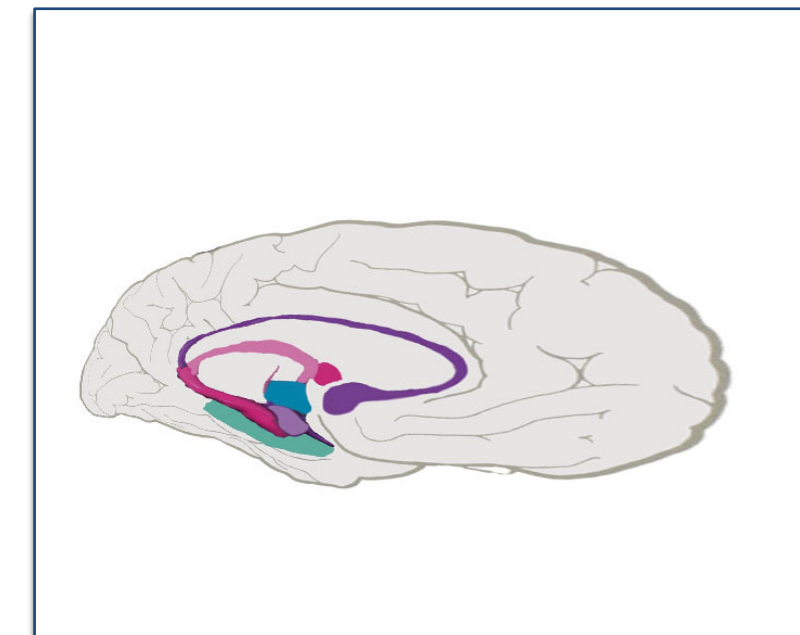
ROTATION



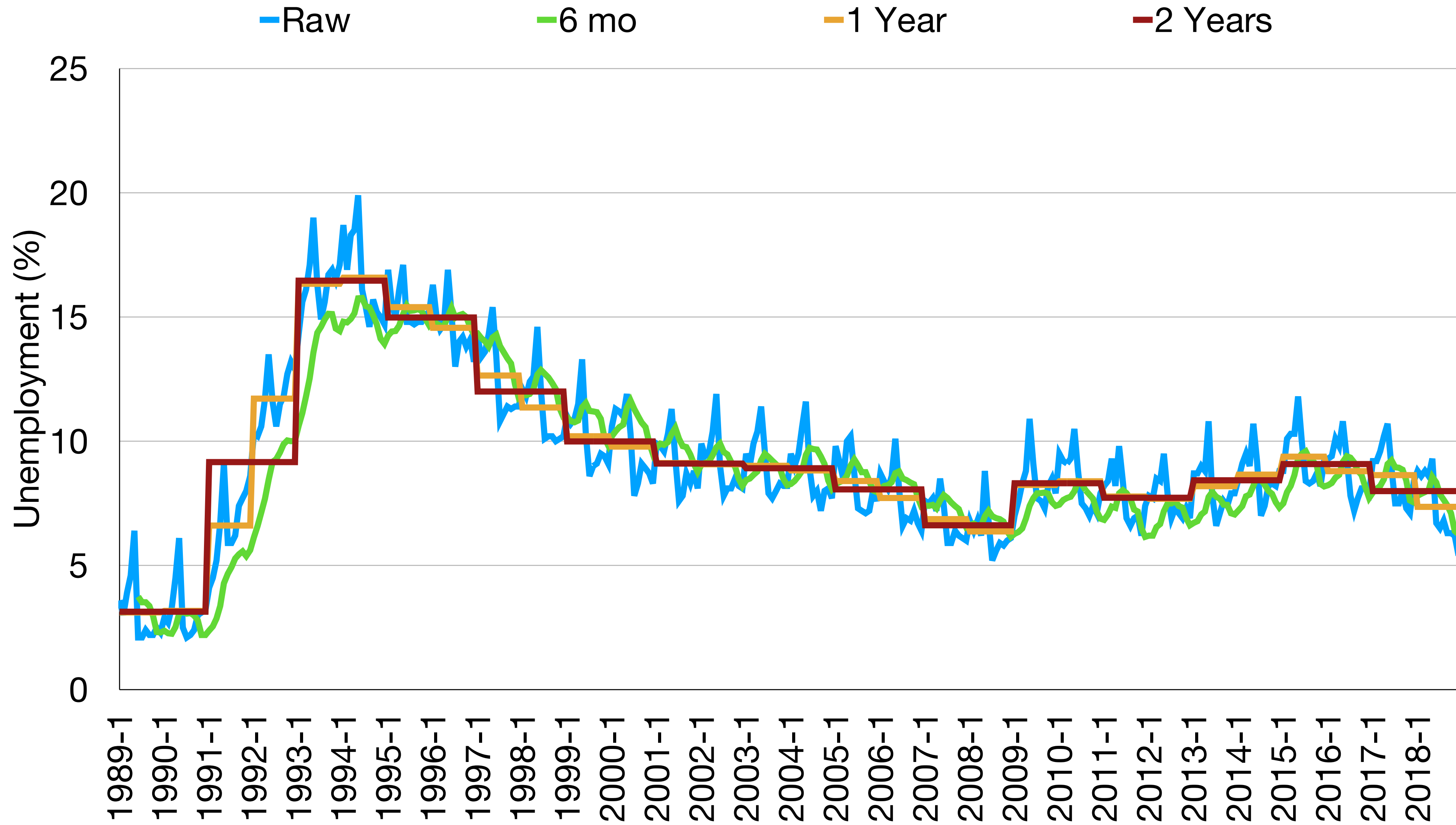
ZOOM



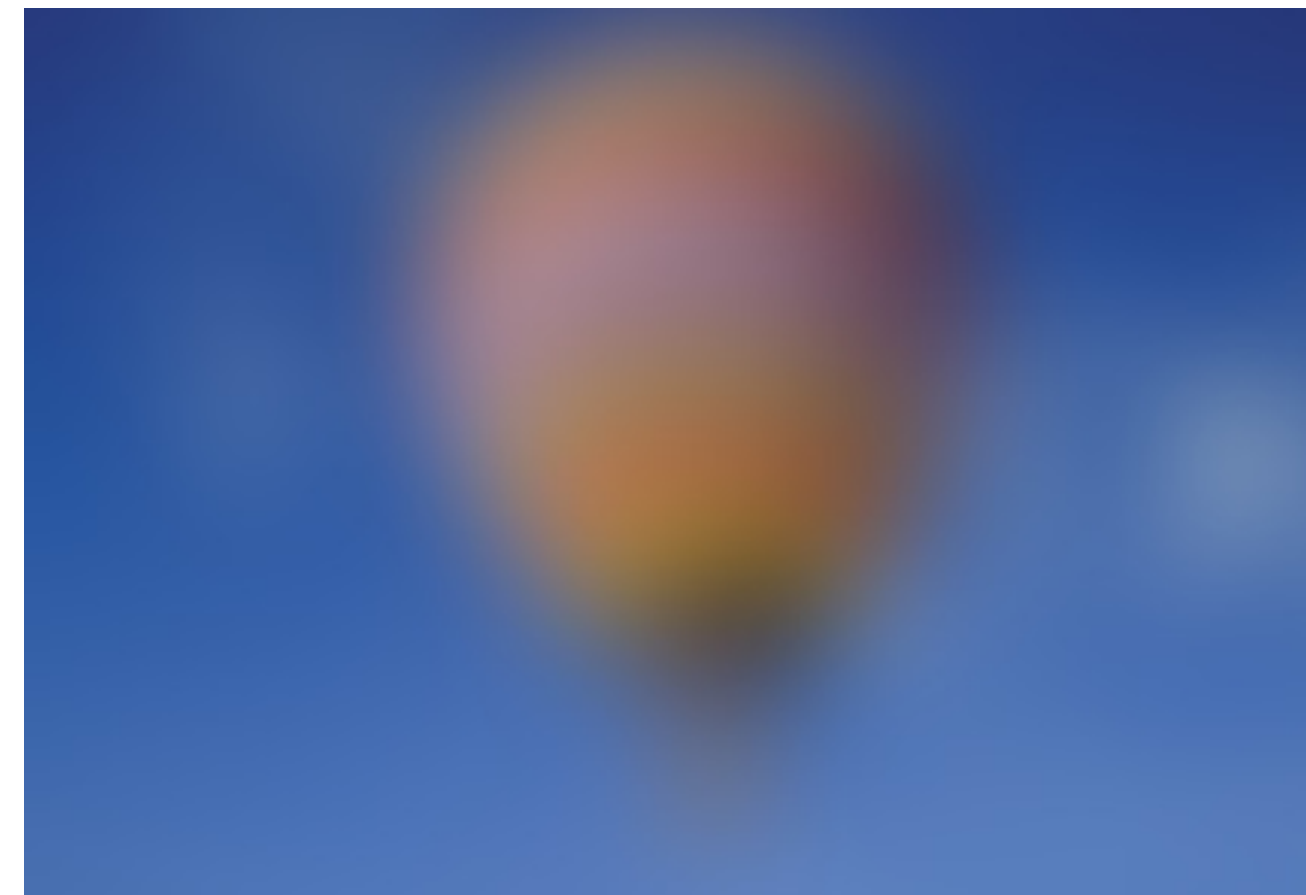
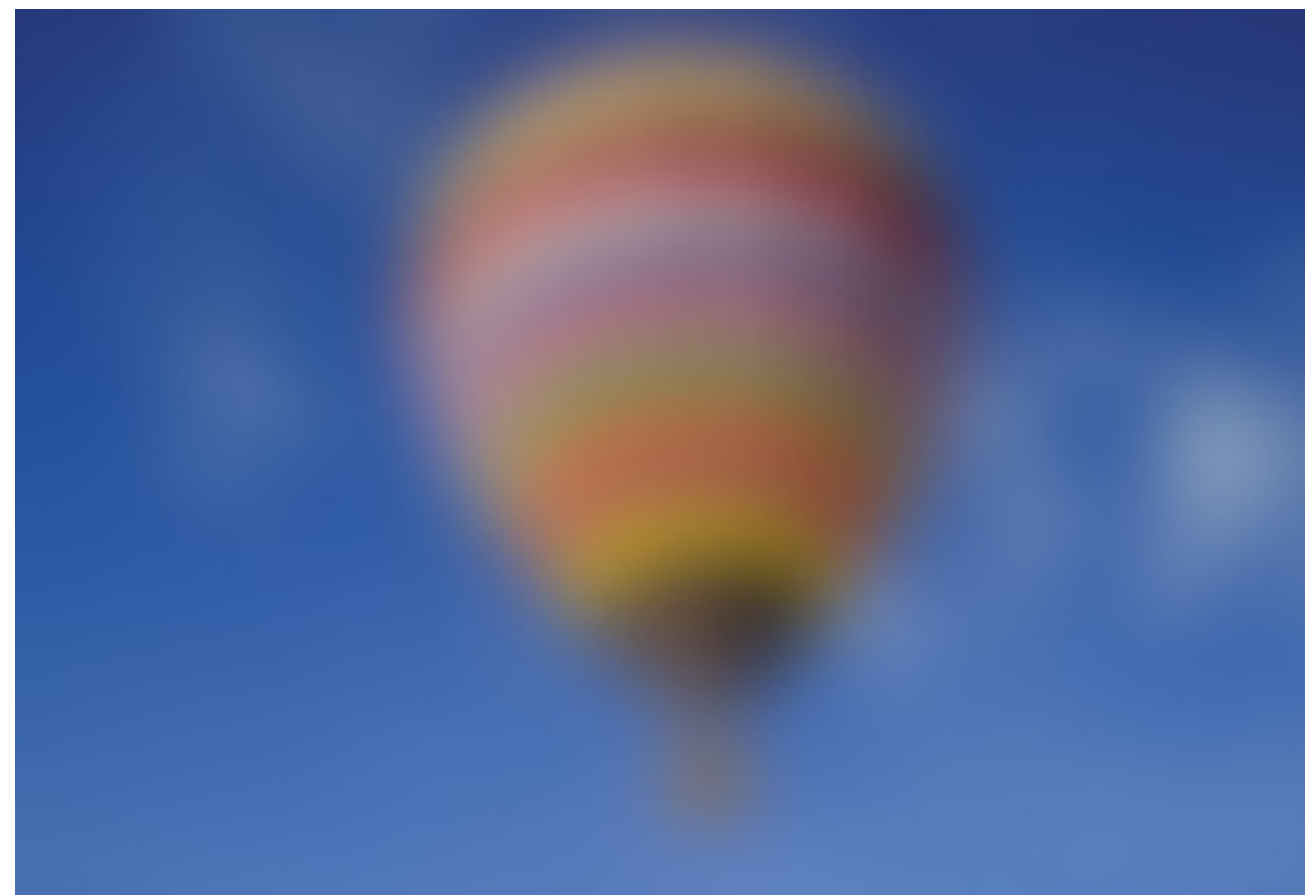
SHEAR



AFFINE NORMALIZATION: 4*3 PARAMETERS



Smoothing



FWHM = spatial extent of the filter

Example on smoothing brain-PET images

UNSMOOTHED



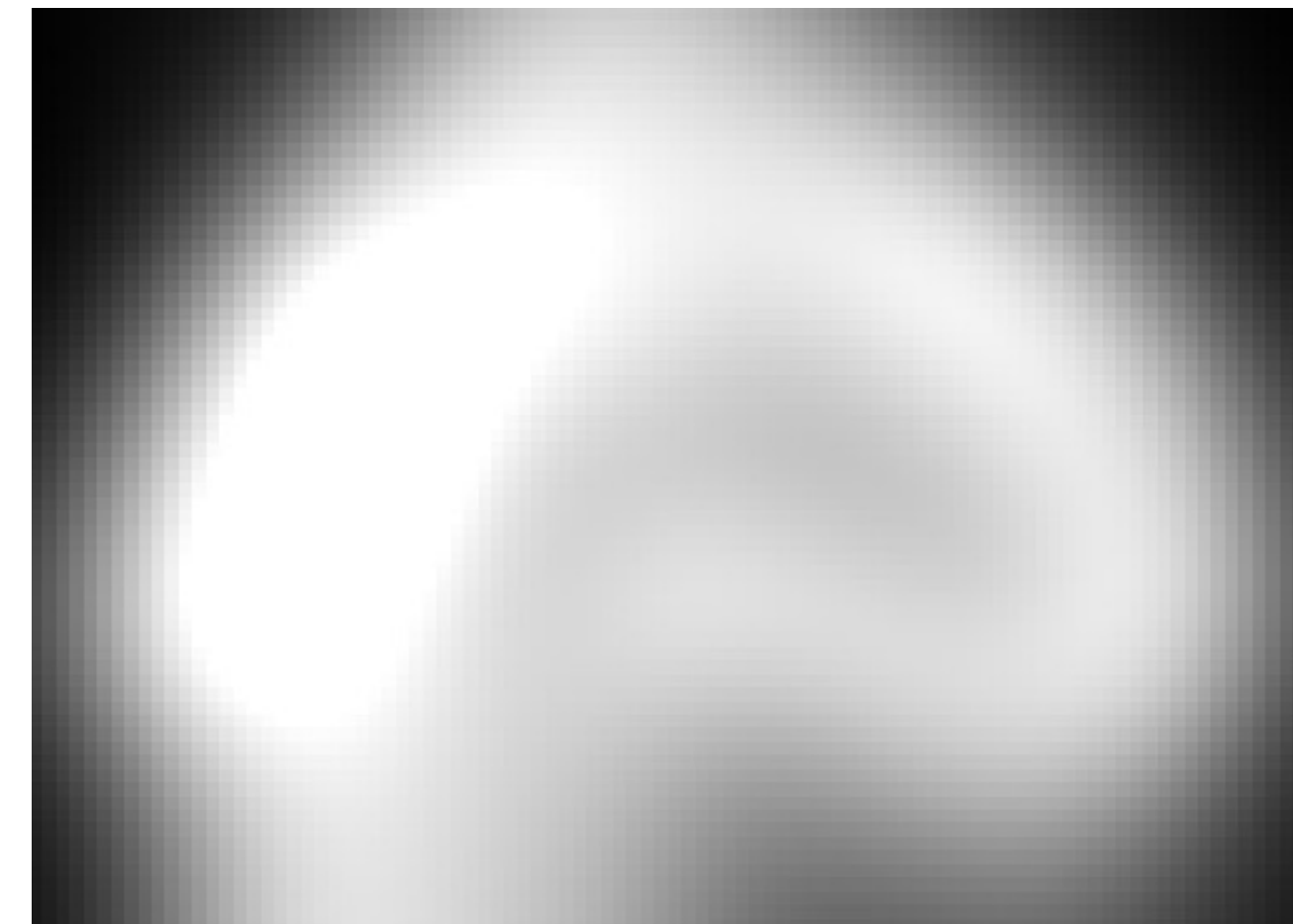
12mm FWHM



16mm FWHM



32mm FWHM

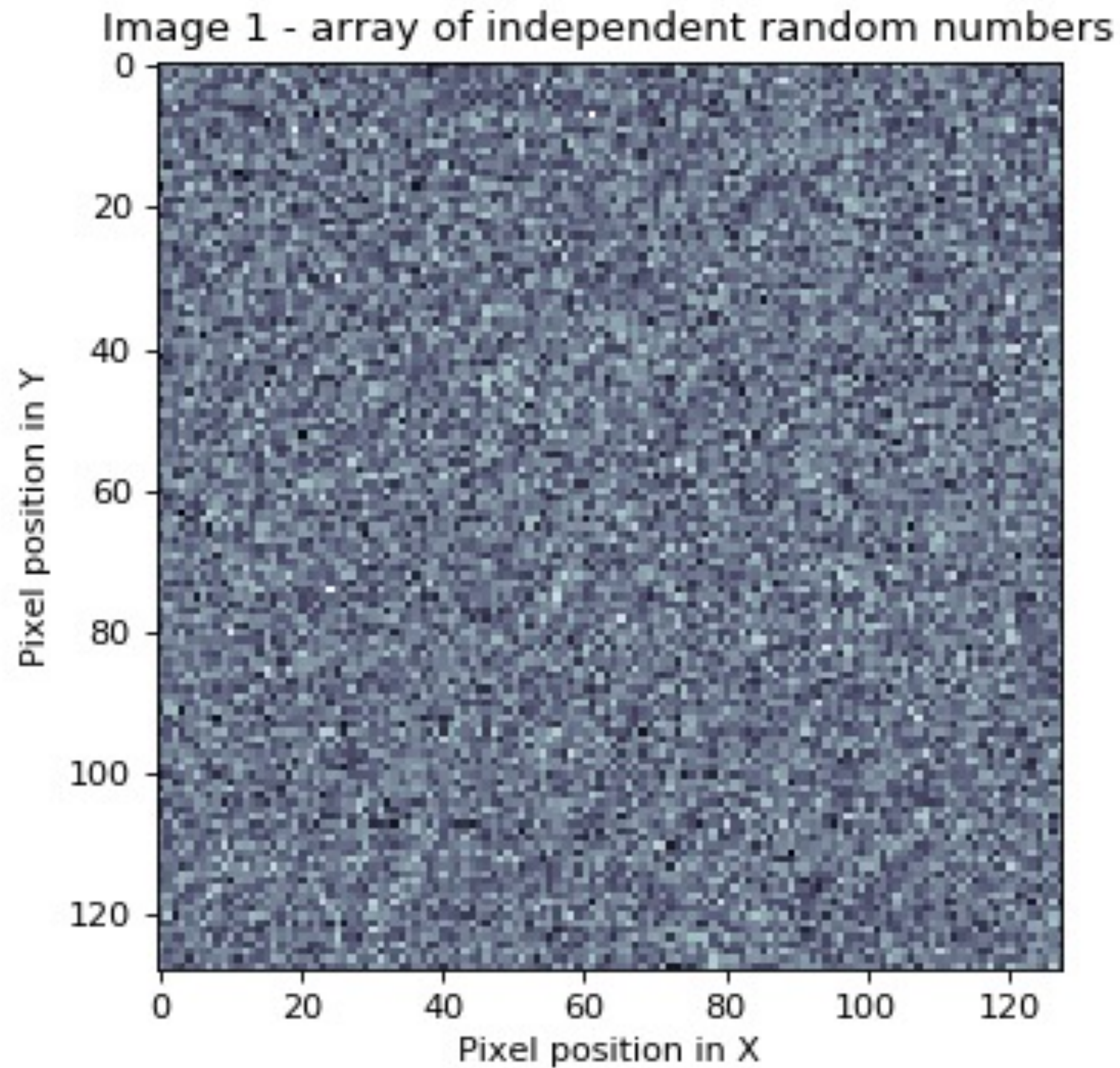


Why smooth?

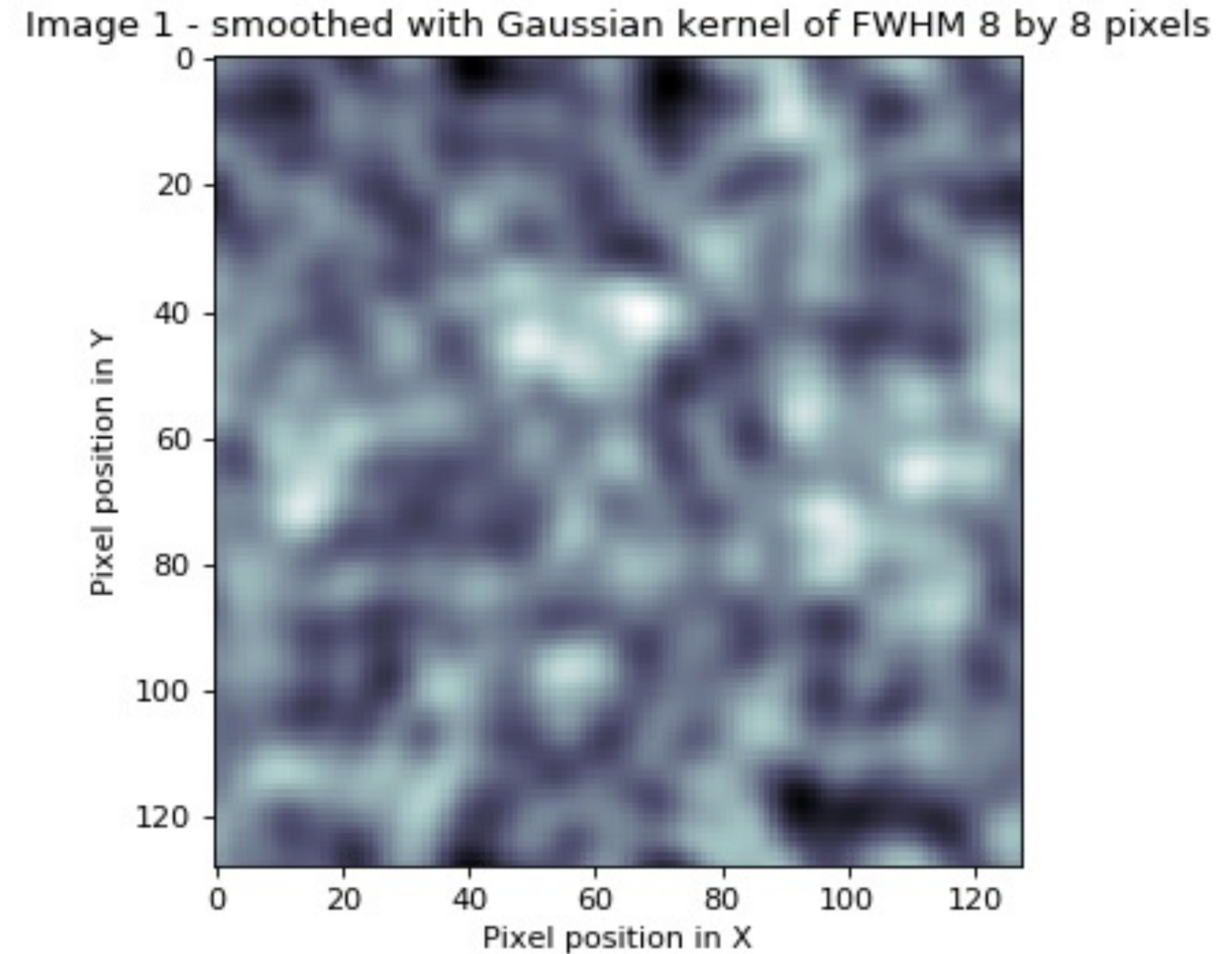
- Smoothing neuroimaging data: reduces noise and anatomical discrepancies
- Assumption: error terms are roughly Gaussian; FWHM greater than voxel size
- Enables hypothesis testing and dealing with multiple comparison problem in functional imaging
- However introduces problem of how to correct for multiple comparisons

Raw data: 16384
independent numbers

Kernel-based smoothing
How many independent numbers?



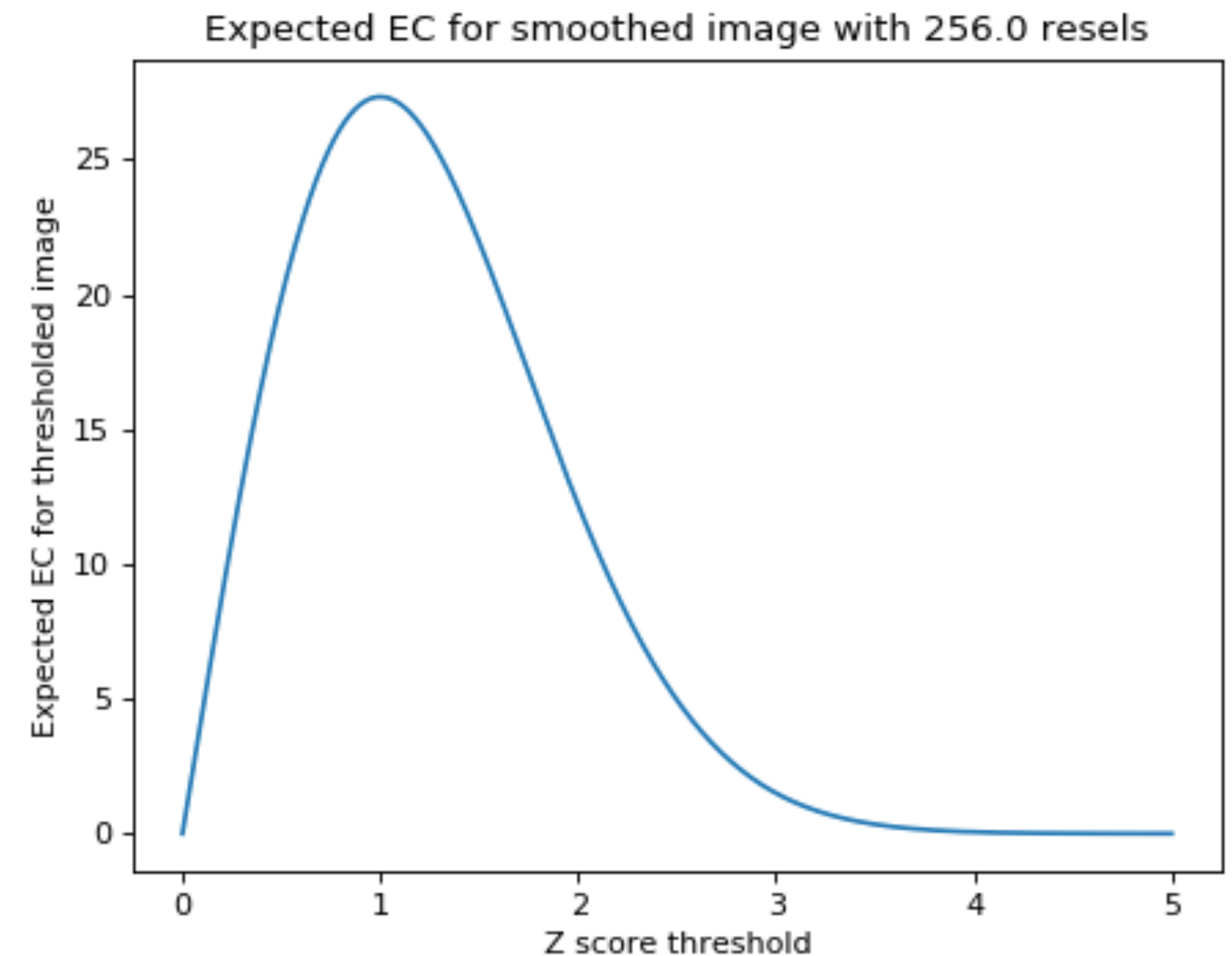
**8 by 8
square
smooth**



Problem with kernel-based smoothing: How many numbers are independent?

Random Field Theory in nutshell

- Estimate the number of resels in the image
 - Resel= block of pixels / voxels of the same size as the FWHM of the smoothness of the image.
Depends on both image size and FWHM
- Work out the Euler characteristic (EC) of the image
 - Property of the image after it has been thresholded.
Roughly number of blobs in image after thresholding
- Resels and EC are linked: when Z thresholds increases and EC drops the expected EC approximates the probability of observing one or more blobs at that threshold.



What sort of voxelwise model to fit?

GLM

ANOVA, ANCOVA, linear regression...

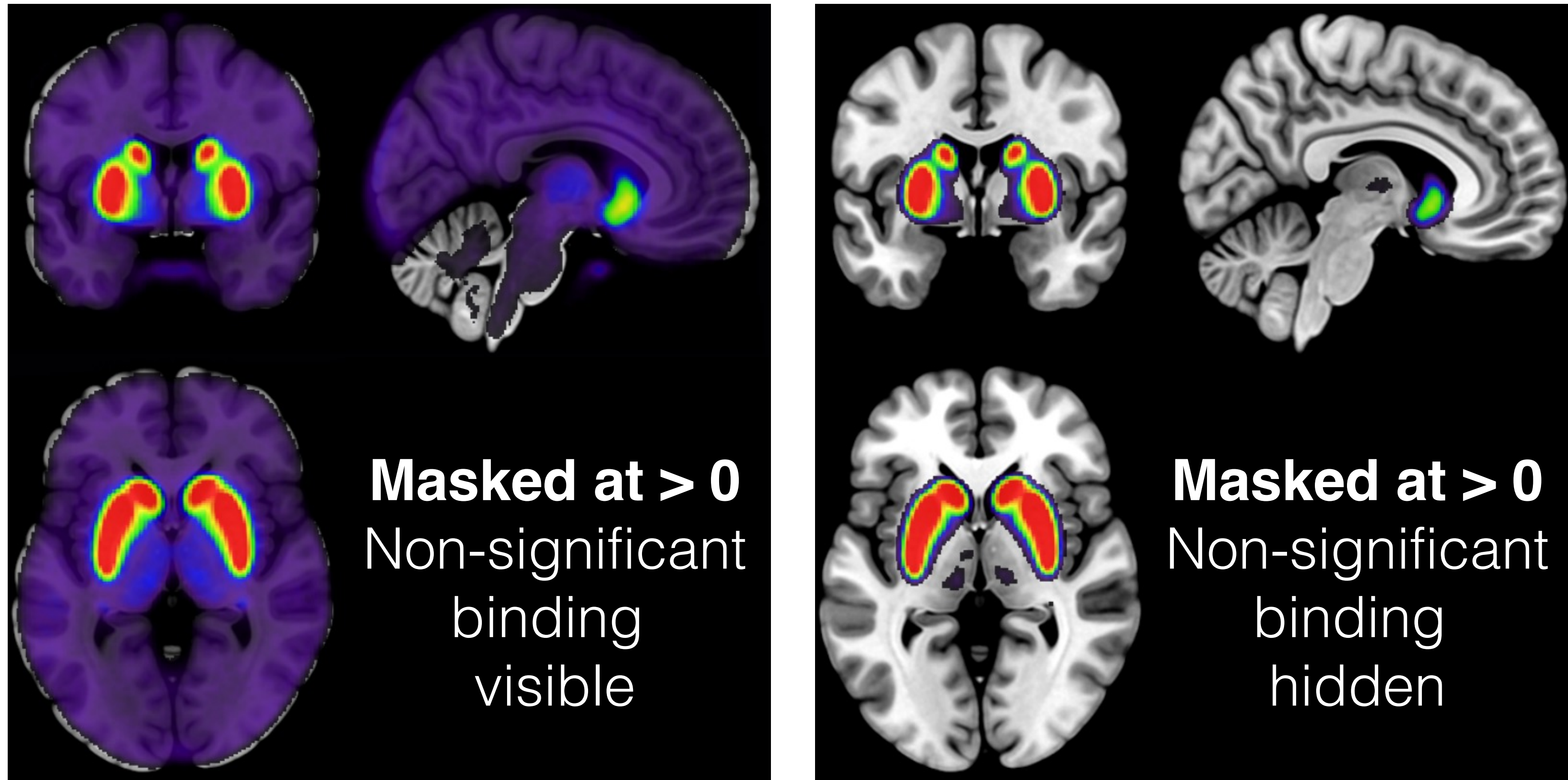
The diagram shows the linear regression equation $Y_i = \beta_0 + \beta_1 X_i + \epsilon_i$ with several labels and arrows pointing to the corresponding terms:

- Dependent Variable** points to Y_i .
- Population Y intercept** points to β_0 .
- Population Slope Coefficient** points to β_1 .
- Independent Variable** points to X_i .
- Random Error term** points to ϵ_i .

Below the equation, two blue brackets indicate the components:

- A bracket under $\beta_0 + \beta_1 X_i$ is labeled **Linear component**.
- A bracket under ϵ_i is labeled **Random Error component**.

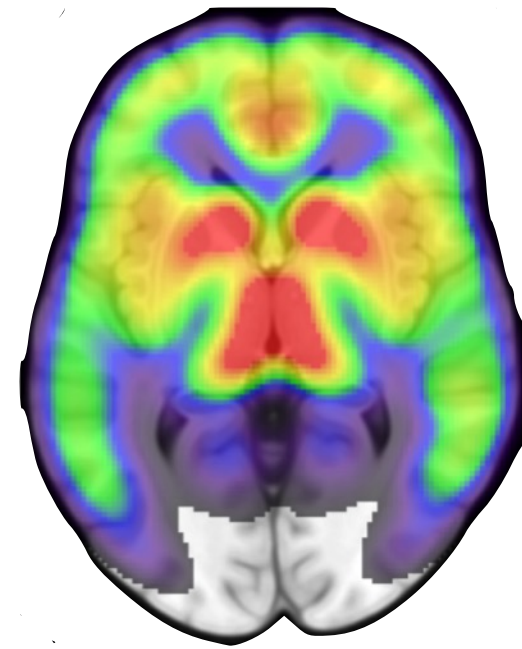
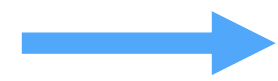
Masking the data



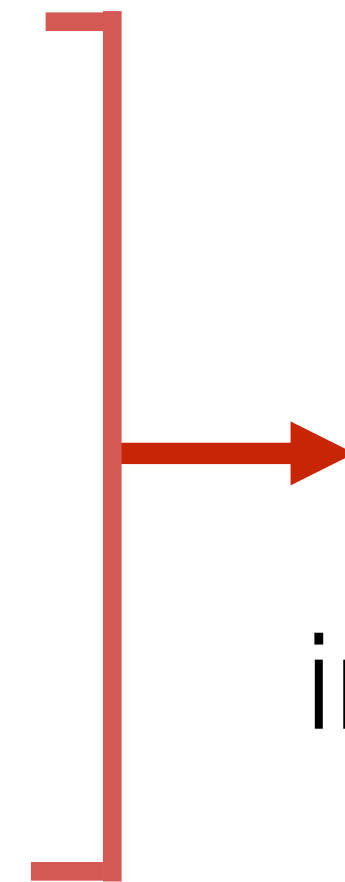
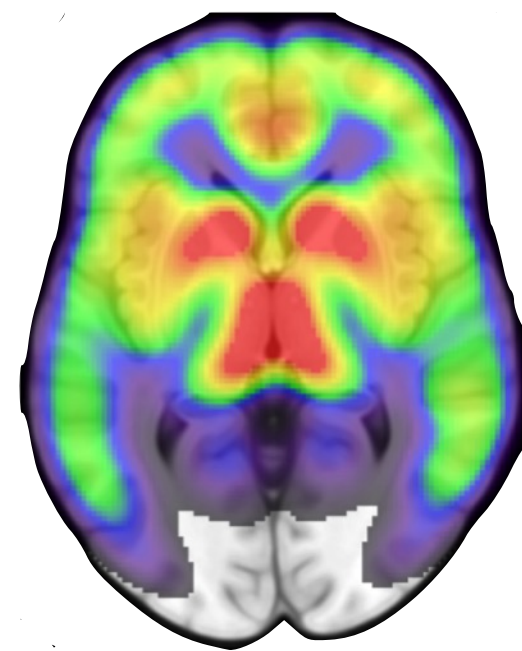
Applying explicit / threshold mask is necessary to avoid fitting model to noise

Between-groups design

Group 1

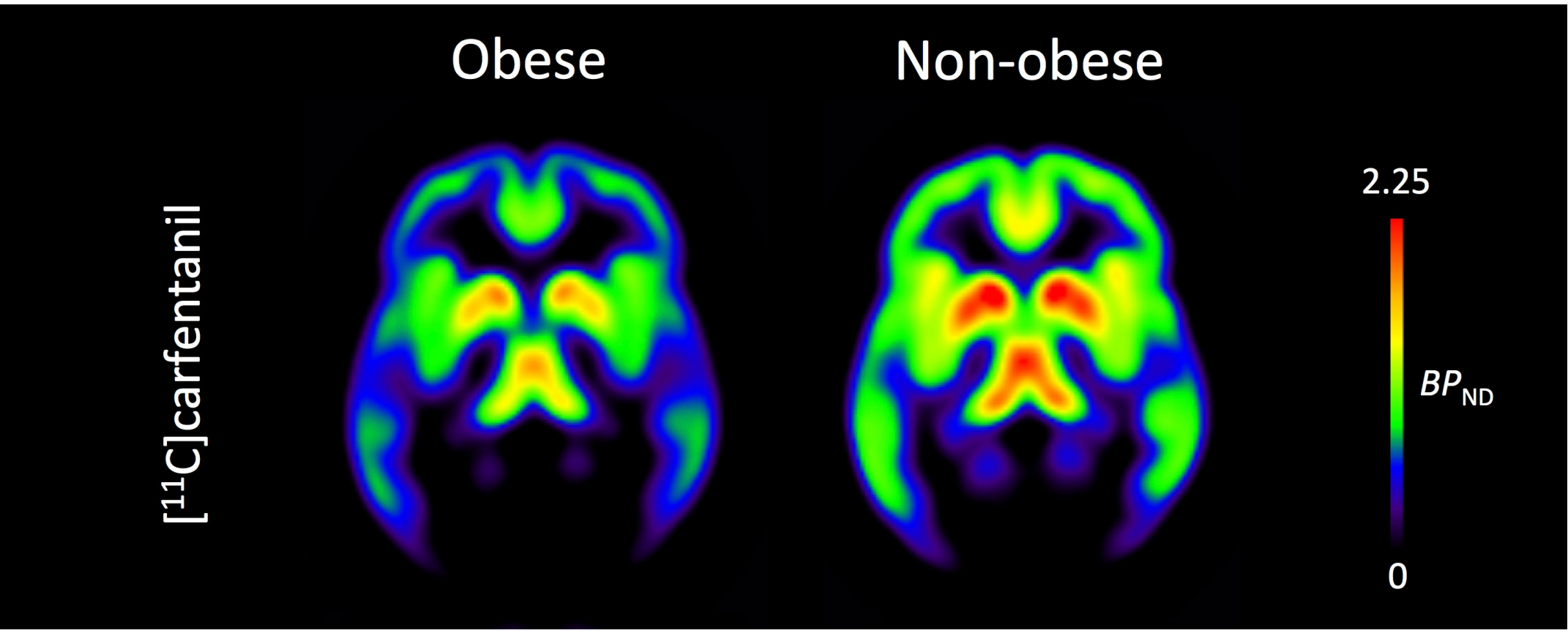


Group 2

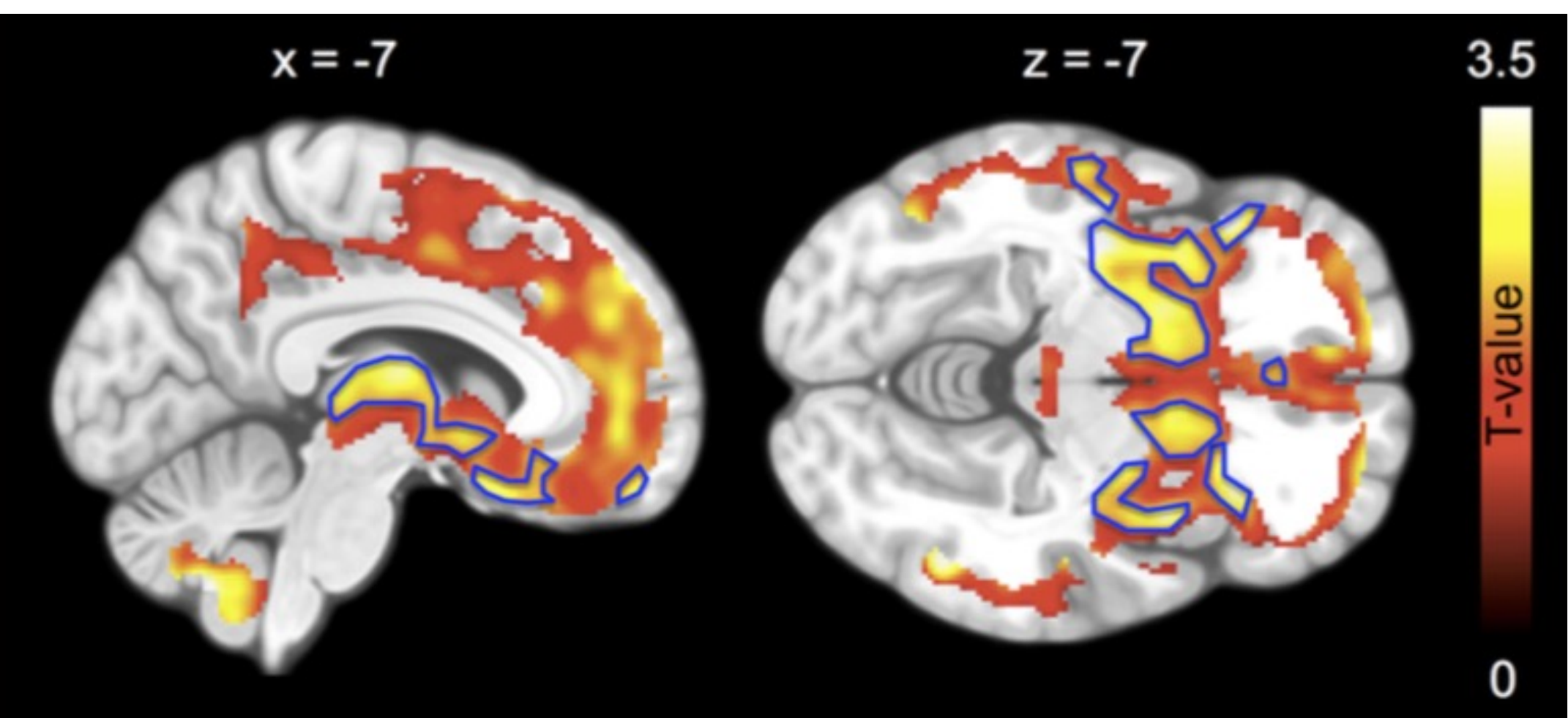


Voxelwise
comparison
with mass univariate
independent samples tests

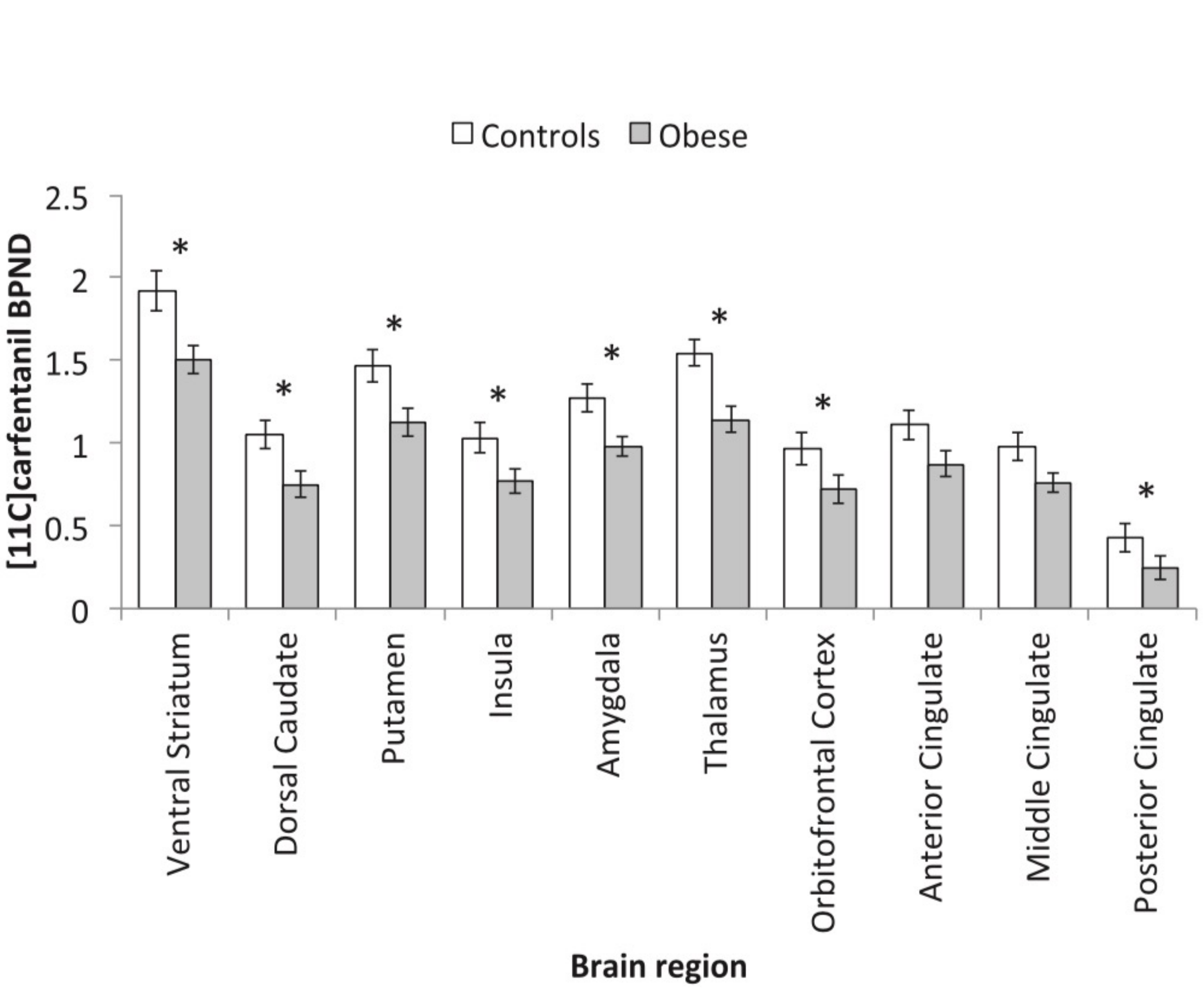
1) Mean images for each group



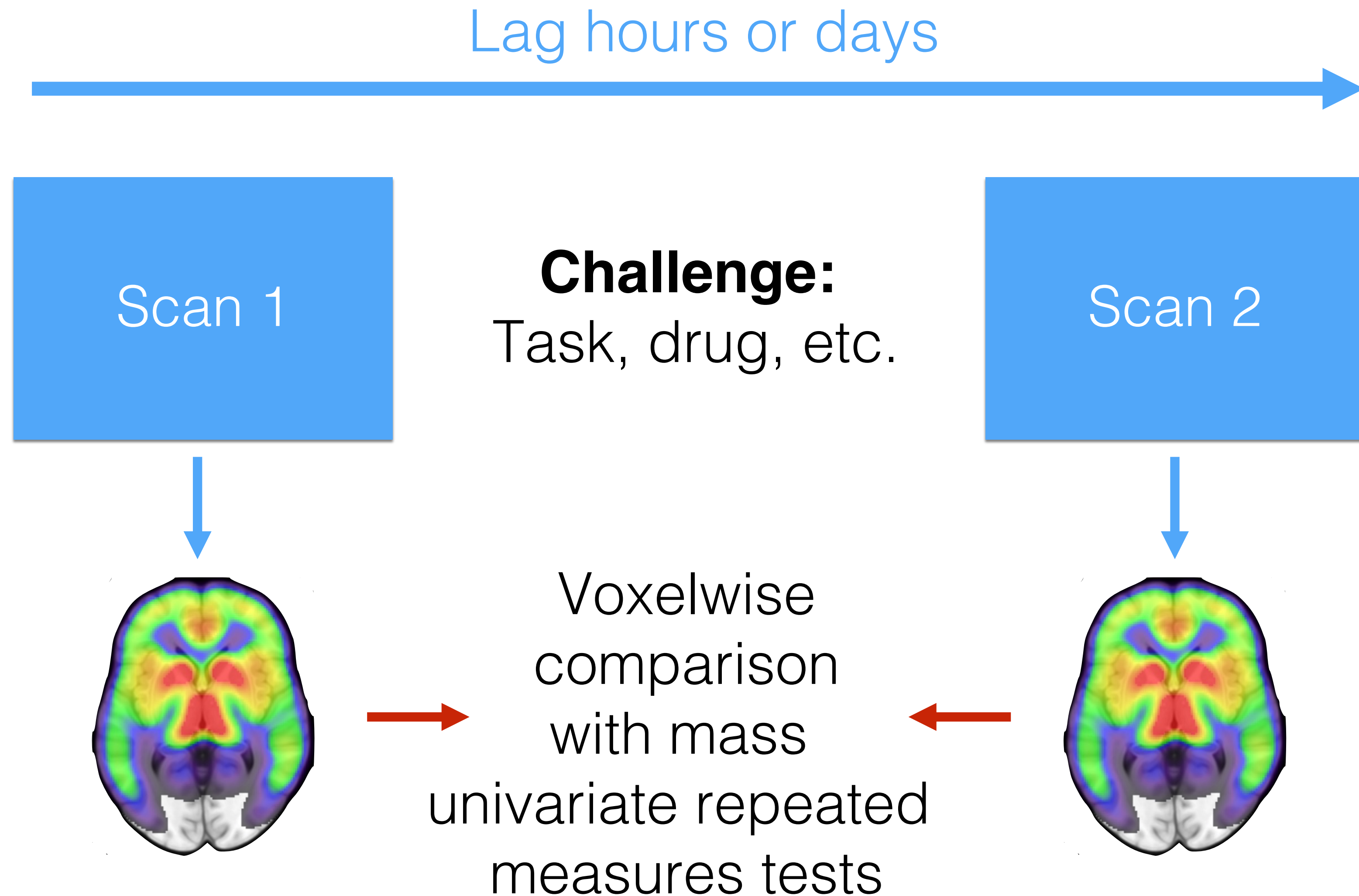
2) Statistical differences (t-map)



3) Region-of-interest data



Challenge / longitudinal design

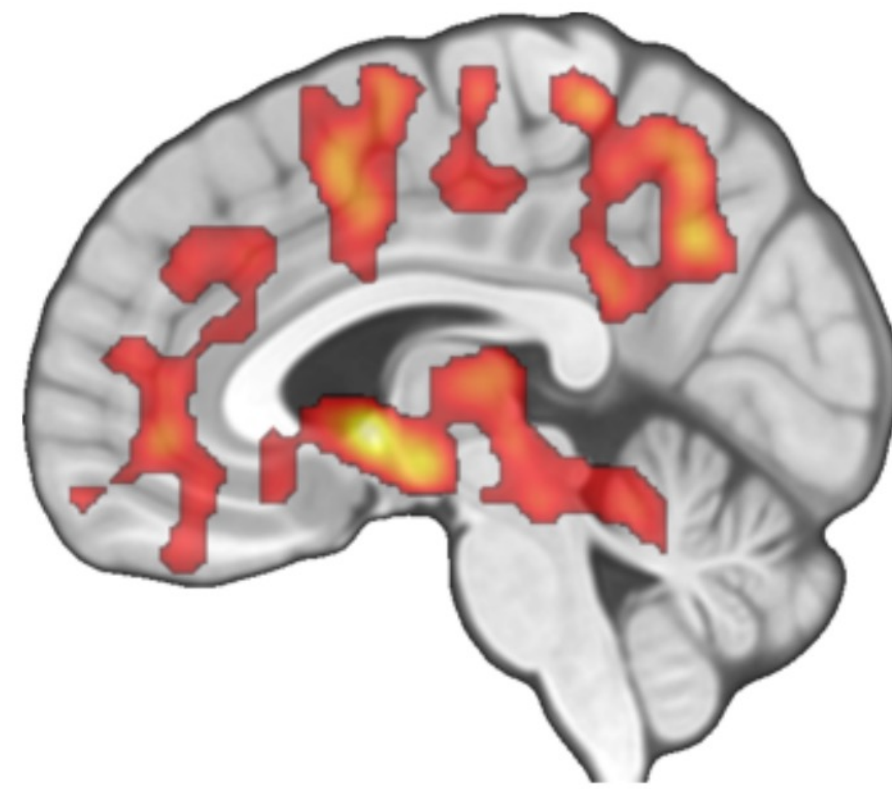
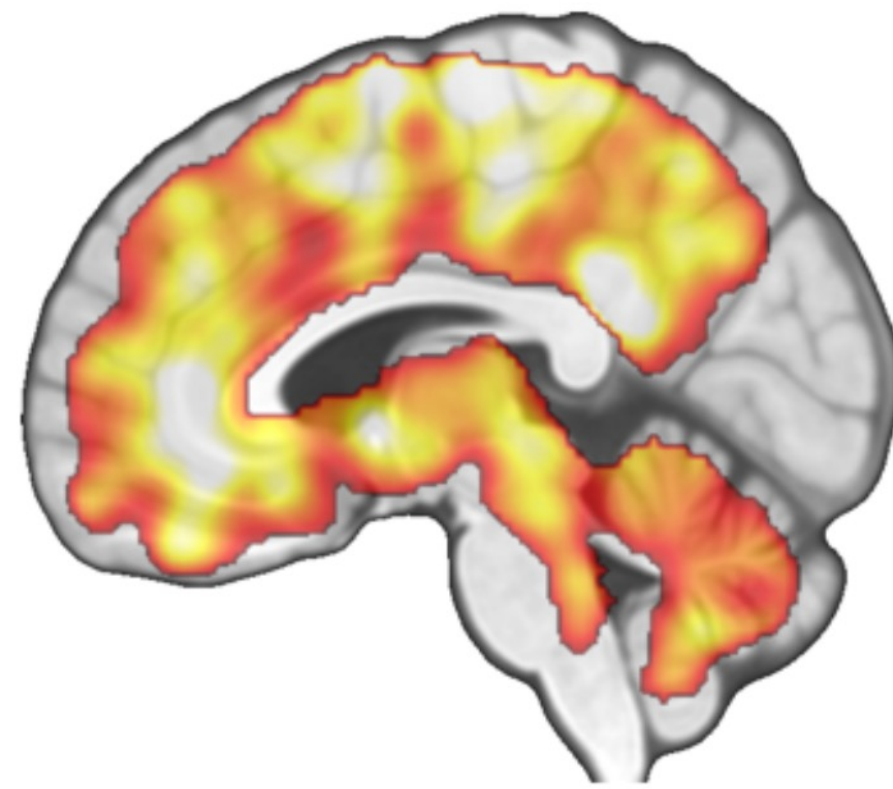


Fast vs.
Non-palatable

Fast vs.
Palatable

□ Non-palatable meal ■ Palatable meal ■ Fast

X = 4

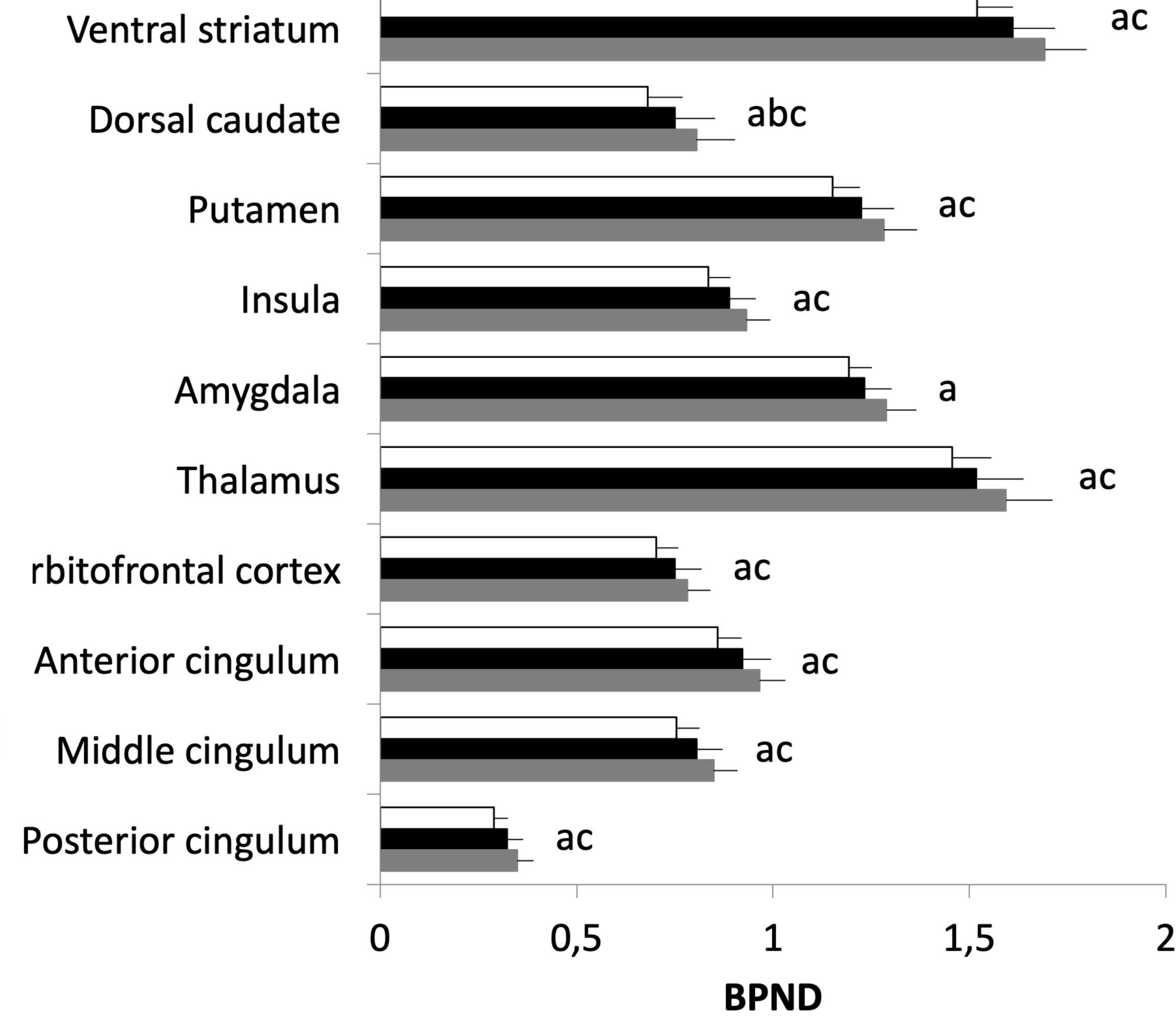
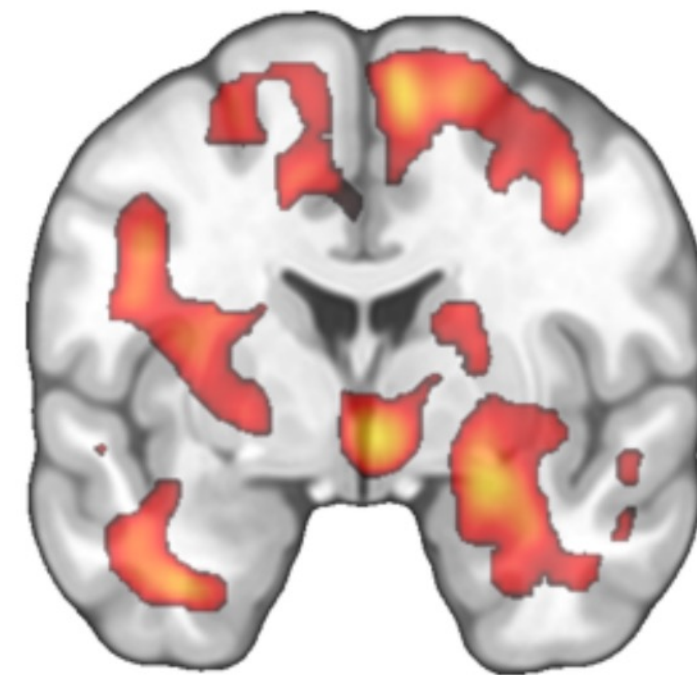
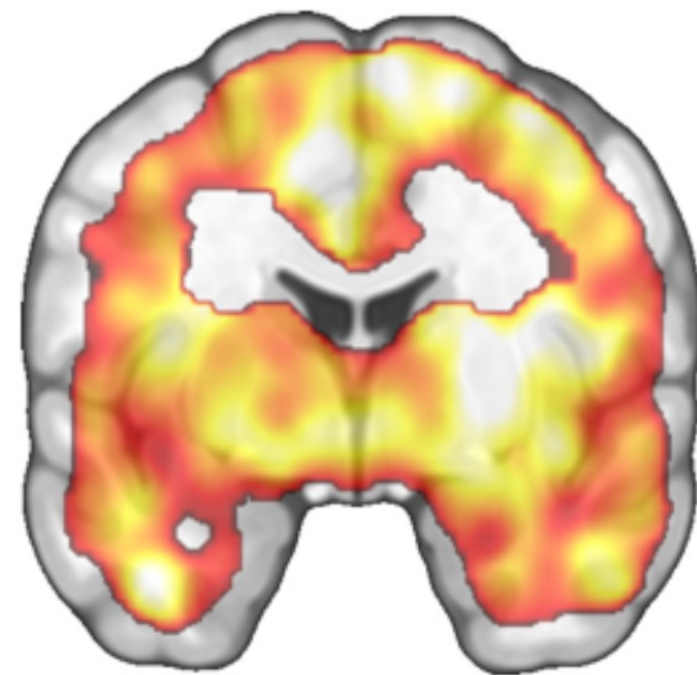


4

T-score

FDR

Y = -1

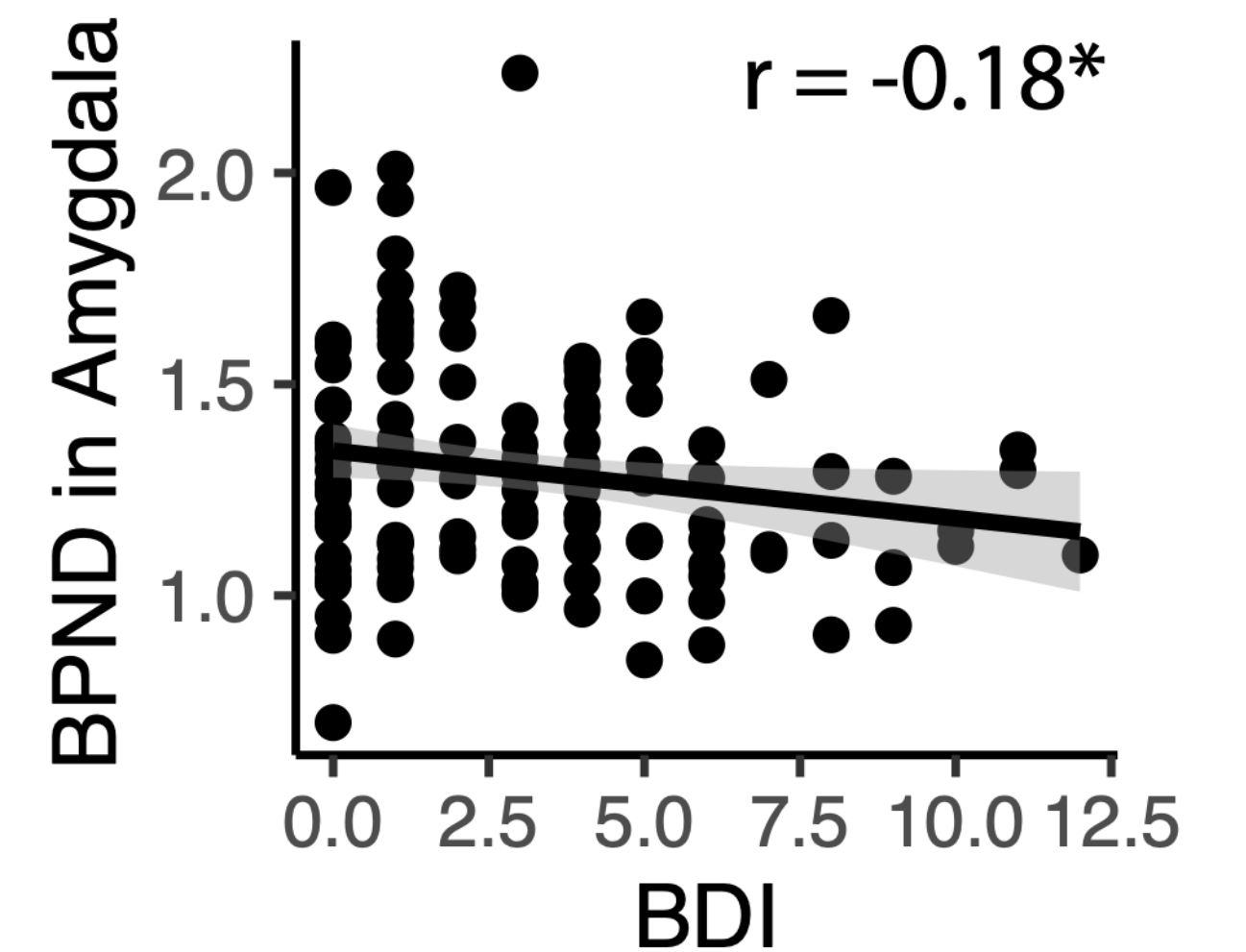
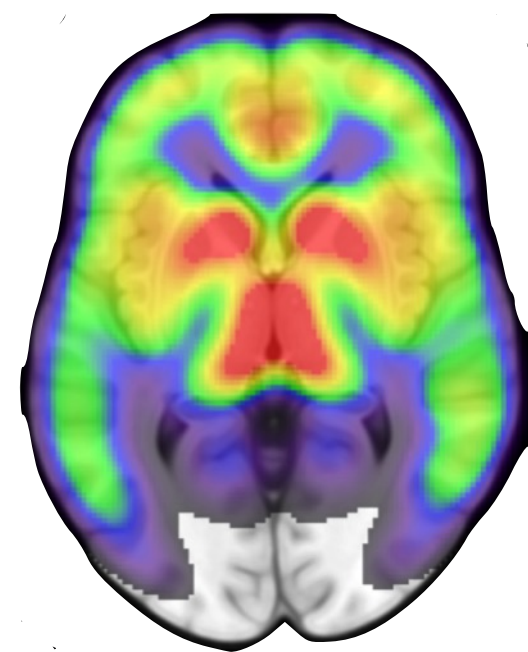


Tuulari et al (2018 J Neurosci)

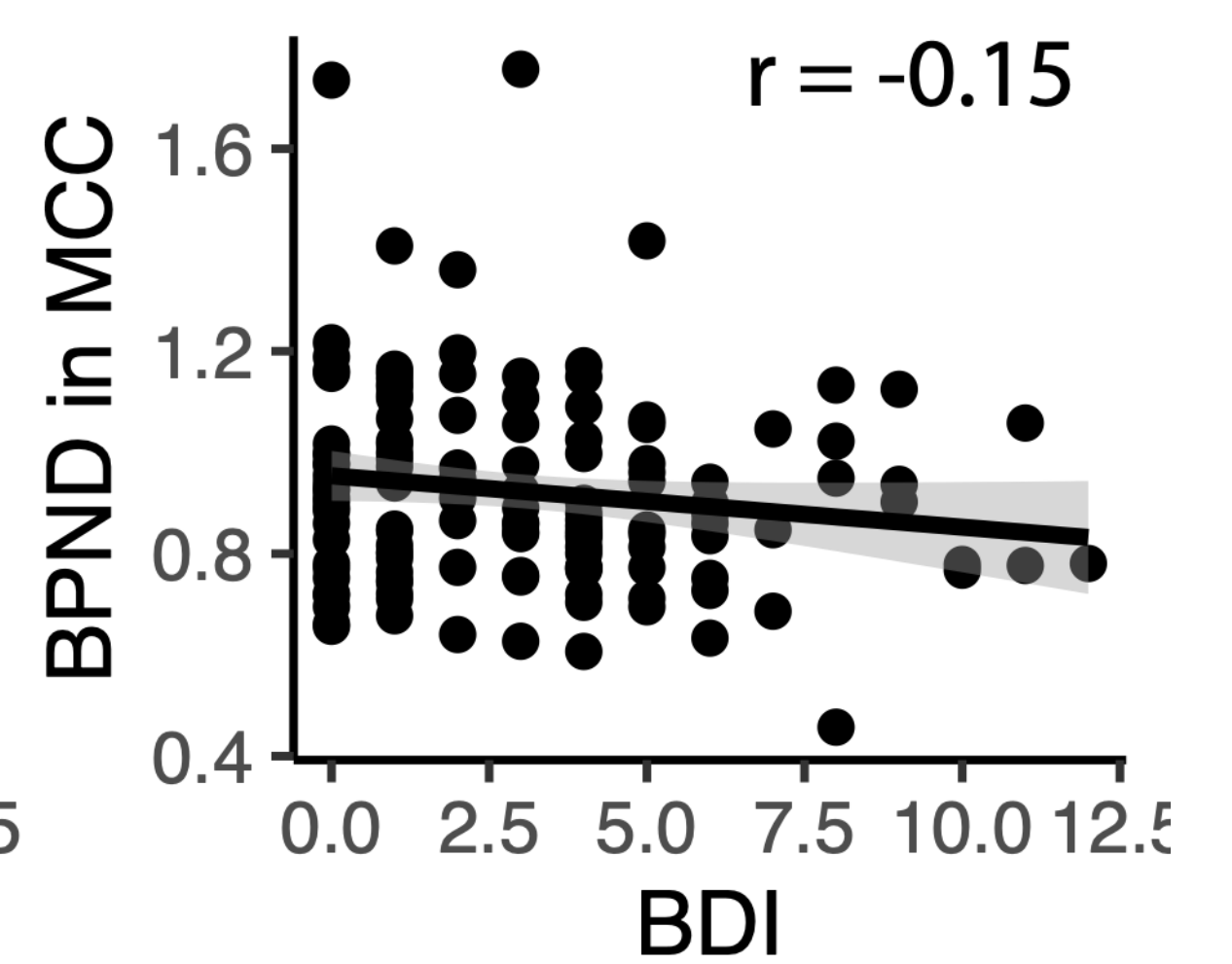
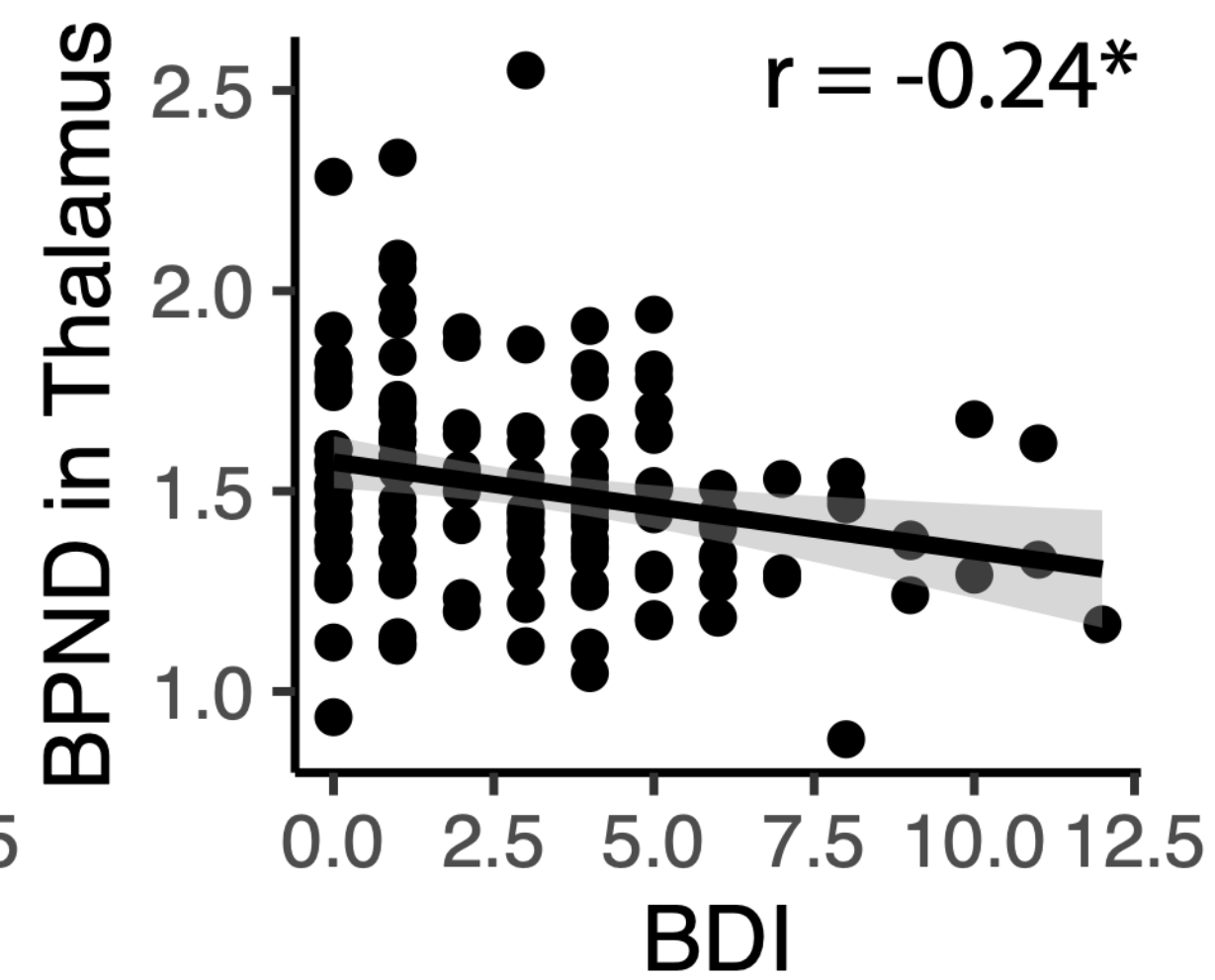
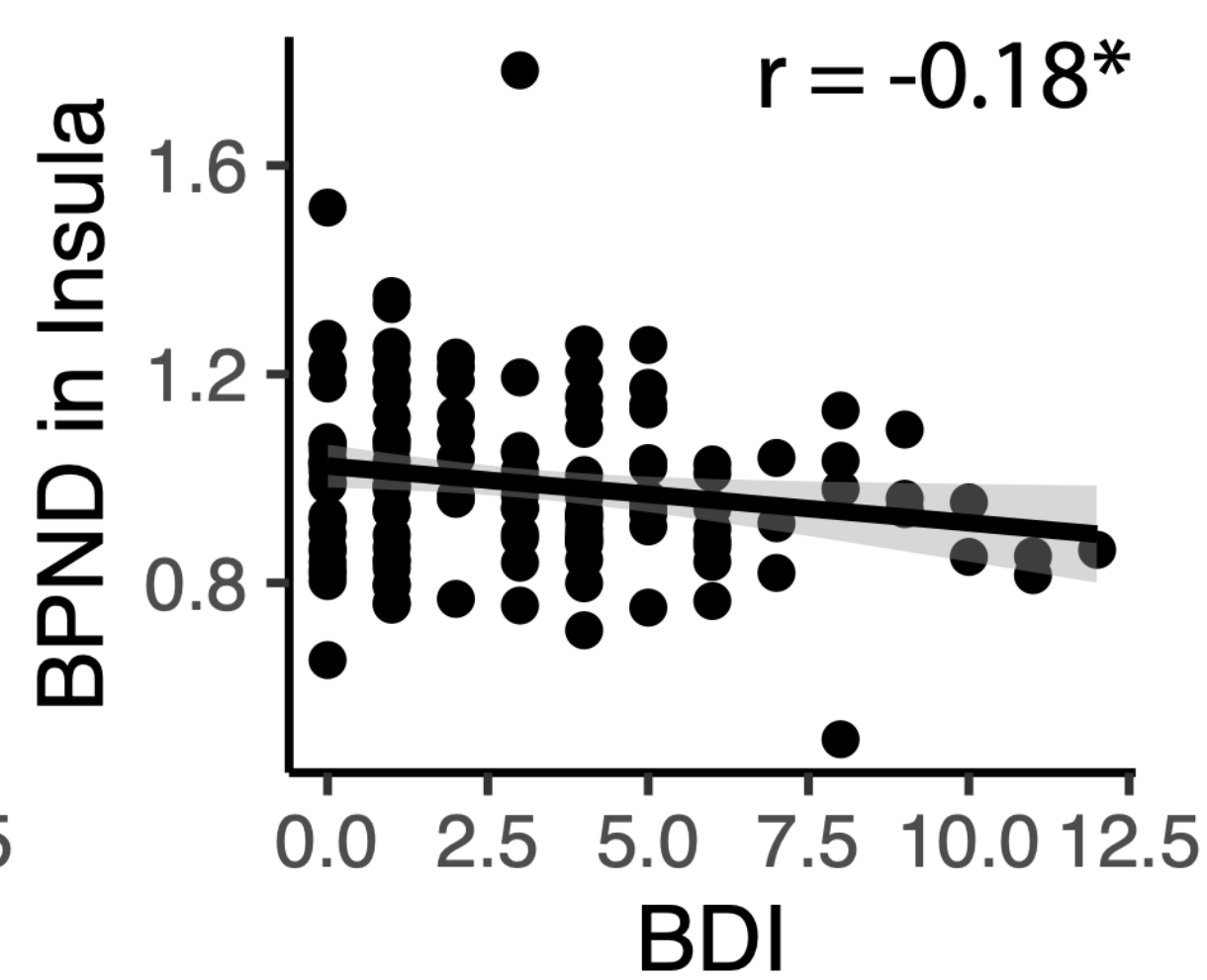
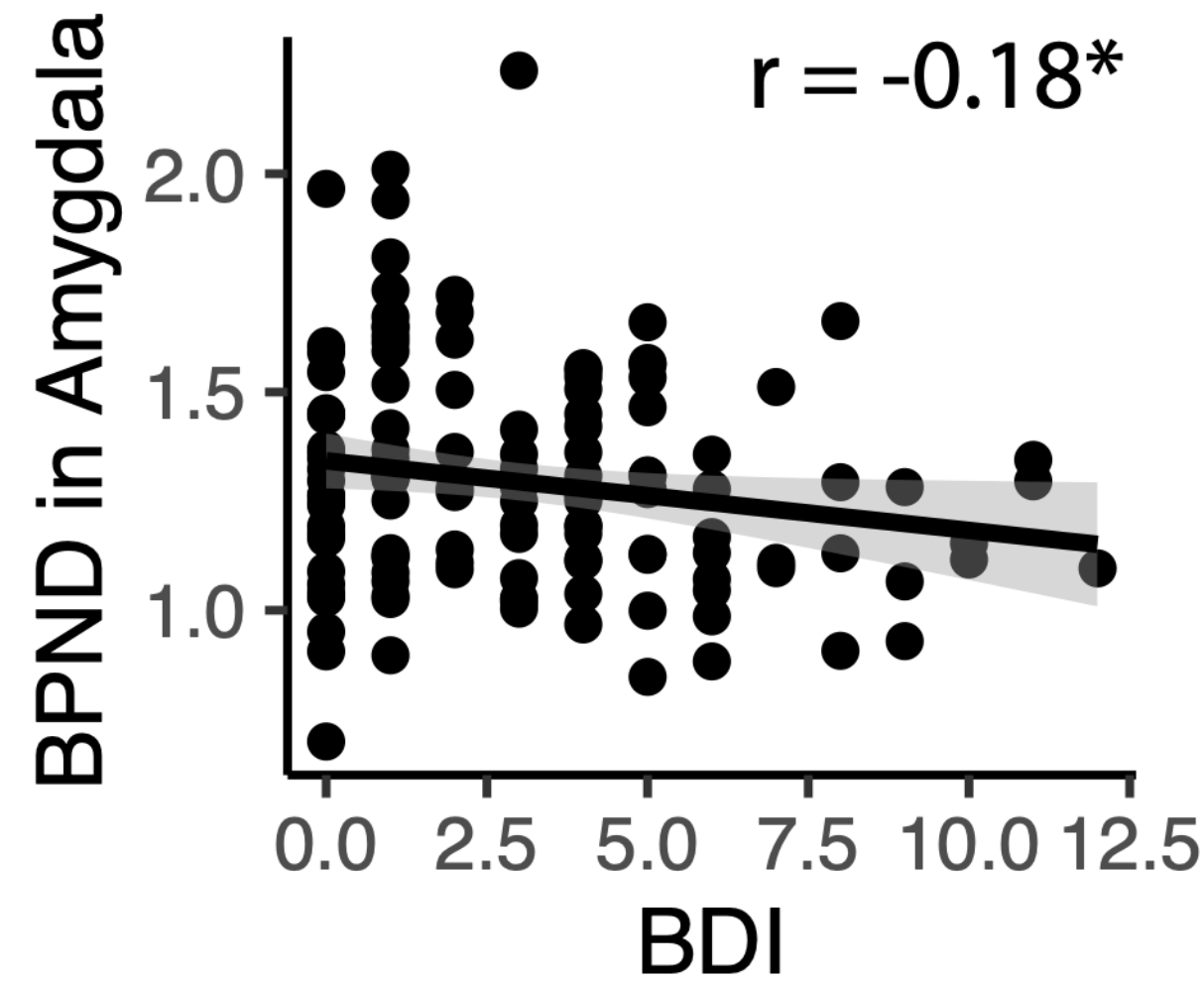
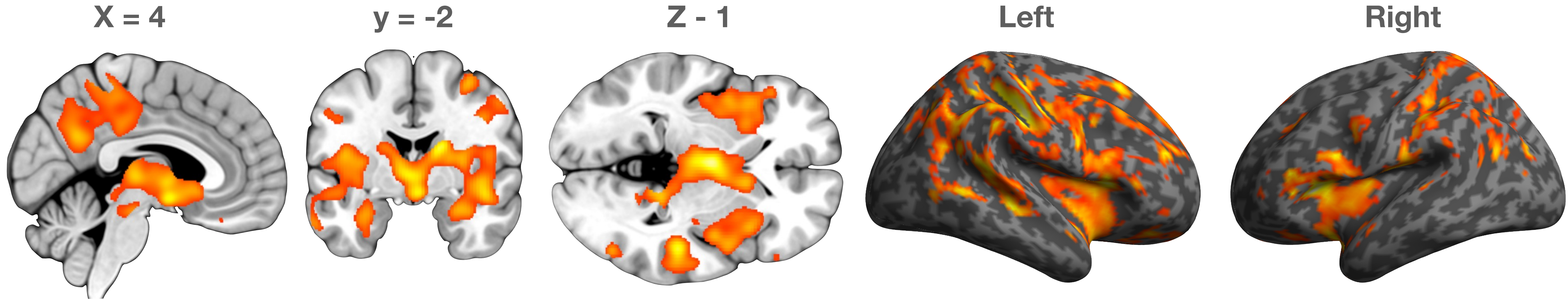
Correlational design

Baseline scan

Univariate biological variable



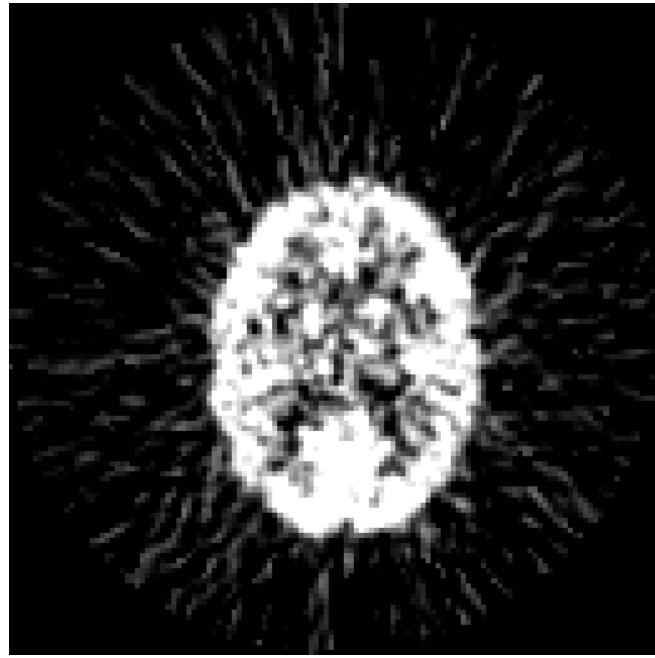
Lowered mu-opioid receptor levels in subclinical depression



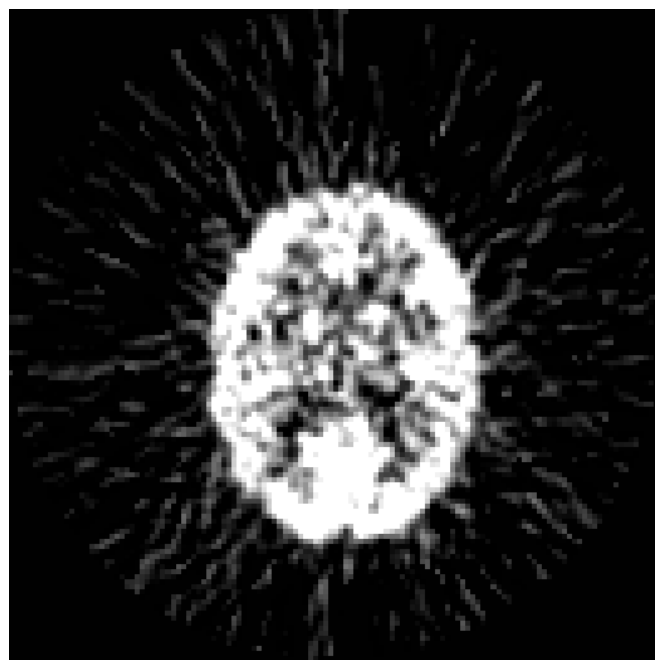
Voxel intensity = outcome measure
(BPND, contrast estimate, tissue probability)

THE BASIC RECIPE

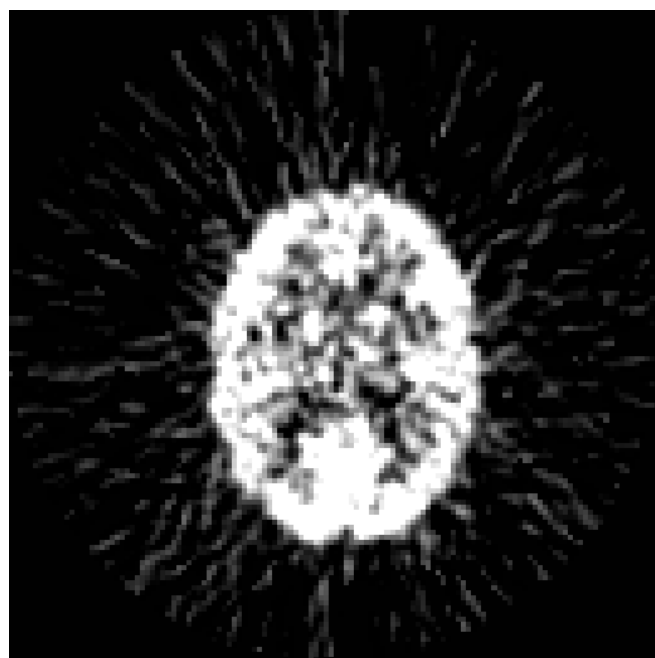
SUBJECT 1



SUBJECT 2

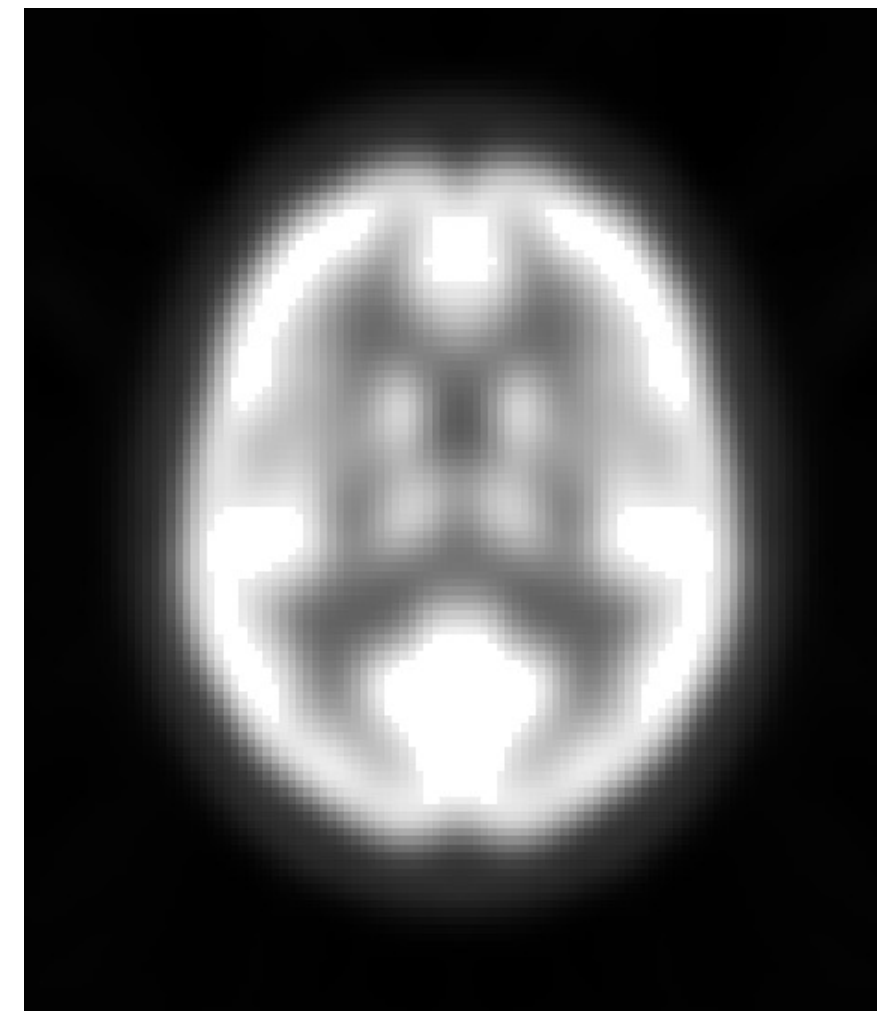


SUBJECT 3



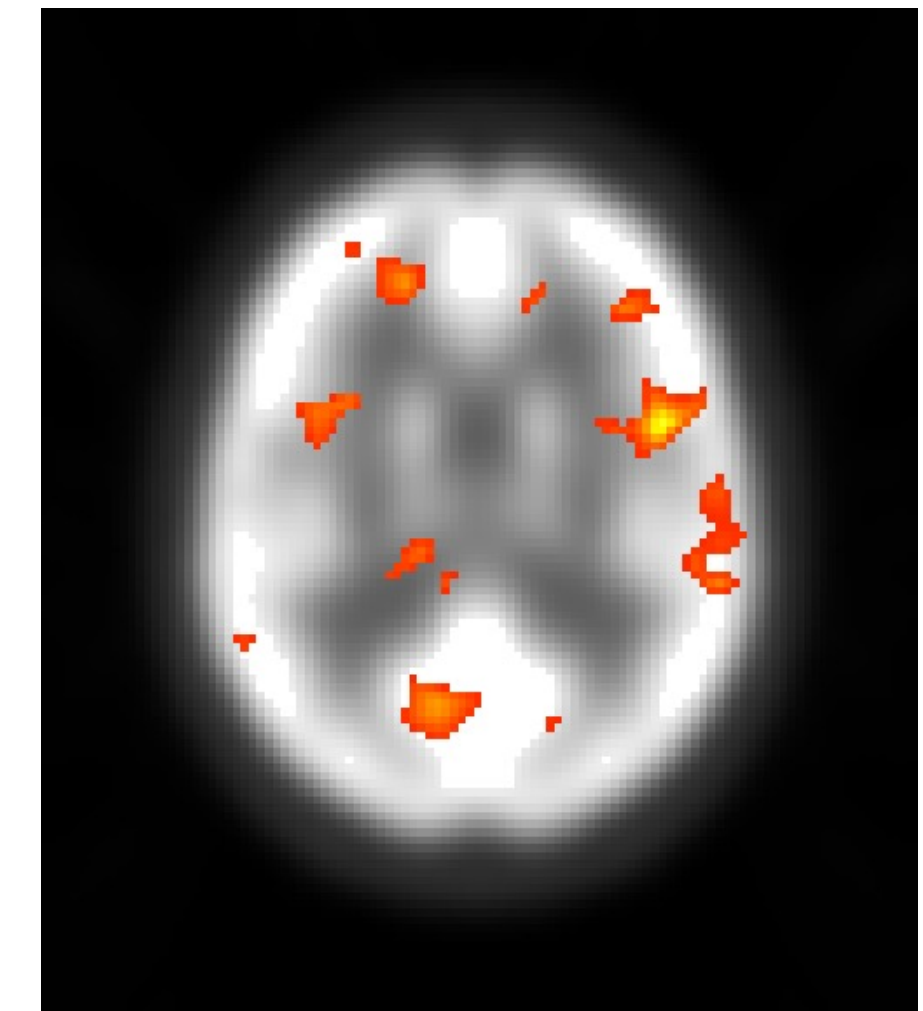
NORMALI-
ZATION

TEMPLATE



GLM

STATISTICAL
PARAMETRIC MAP



SMOOTH

